



Accurate characterization of pure silicon-substituted hydroxyapatite powders synthesized by a new precipitation route

David Marchat, Maria Zymelka, Cristina Coelho, Laurent Gremillard, Lucile Joly-Pottuz, Florence Babonneau, Claude Esnouf, Jérôme Chevalier, Didier Bernache-Assollant

► To cite this version:

David Marchat, Maria Zymelka, Cristina Coelho, Laurent Gremillard, Lucile Joly-Pottuz, et al.. Accurate characterization of pure silicon-substituted hydroxyapatite powders synthesized by a new precipitation route. *Acta Materialia*, 2013, 9 (6), pp.6992-7004. 10.1016/j.actbio.2013.03.011 . hal-00835892

HAL Id: hal-00835892

<https://hal.science/hal-00835892>

Submitted on 20 Jun 2013

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

**Accurate characterization of pure silicon-substituted hydroxyapatite powders
synthesized by a new precipitation route**

David MARCHAT^{1*}, Maria ZYMELKA¹, Cristina COELHO², Laurent GREMILLARD³,
Lucile JOLY-POTTUZ³, Florence BABONNEAU⁴, Claude ESNOUF³, Jérôme
CHEVALIER³, Didier BERNACHE-ASSOLLANT¹

¹ Ecole Nationale Supérieure des Mines, CIS-EMSE, CNRS:FRE3312, F-42023 158 cours
Fauriel Saint-Etienne cedex 2

² Institut des Matériaux de Paris Centre, FR 2482, Université Pierre et Marie Curie and CNRS
Collège de France, 11 place Marcelin Berthelot 75005 Paris, France

³ Université de Lyon, INSA-Lyon, MATEIS Laboratory UMR CNRS 5510, Villeurbanne F-
69621, France

⁴ Laboratoire de Chimie de la Matière Condensée de Paris, CNRS, Université Pierre et Marie
Curie and CNRS, Collège de France, 11 place Marcelin Berthelot 75005 Paris, France.

E-mail addresses : marchat@emse.fr (David Marchat)*, mzymelka@emse.fr (Maria
Zymelka), cristina.coelho@upmc.fr (Cristina Coelho), laurent.gremillard@insa-lyon.fr
(Laurent Gremillard), lucile.joly-pottuz@insa-lyon.fr (Lucile Joly-Pottuz),
florence.babonneau@upmc.fr (Florence Babonneau), claud.e.snouf@insa-lyon.fr (Claude
Esnouf), jerome.chevalier@insa-lyon.fr (Jérôme Chevalier), bernache@emse.fr (Didier
Bernache-Assollant),

*Corresponding author: Phone: 0033 (0)4 77 49 97 01, Fax: 0033 (0)4 77 49 96 94

Address: Ecole Nationale Supérieure des Mines, Centre Ingénierie et Santé, 158 cours
Fauriel 42023 Saint-Etienne, cedex 2, France.

Abstract

This paper presents a new aqueous precipitation method to prepare silicon-substituted hydroxyapatites $\text{Ca}_{10}(\text{PO}_4)_6\text{-(SiO}_4)_y(\text{OH})_{2-y}(\text{VOH})_y$ (SiHAs) and details the characterization of powders with varying Si content up to $y=1.25 \text{ mol mol}_{\text{SiHA}}^{-1}$. X-ray diffraction (XRD), transmission electron microscopy (TEM), solid-state nuclear magnetic resonance (NMR) and Fourier transform infrared (FTIR) spectroscopy were used to accurately characterize samples calcined at 400°C for 2 h and 1000°C for 15 h. This method allows for synthesizing monophasic SiHAs with controlled stoichiometry. The theoretical maximum limit of incorporation of Si into the hexagonal apatitic structure is $y<1.5$. This limit depends on the OH content in the channel, which is a function of the Si content, temperature and atmosphere of calcination. These results, particularly those from infrared spectroscopy, express serious reservations about the phase purity of SiHA powders, pellets or scaffolds prepared and biologically evaluated in the literature.

Keywords: biomaterials; silicon-substituted hydroxyapatite; precipitation method, infrared spectroscopy, NMR spectroscopy.

1. Introduction

According to the literature, silicon-substituted hydroxyapatite (SiHA) is a highly promising material in the field of bioactive bone substitutes and bone tissue engineering. It is now well-established that silicon plays an important role in the early stage of cartilage and bone growth [1-4]. Soluble silicon species have been shown to stimulate spontaneous calcium phosphate precipitation (*i.e.* the mineral bone phase) [5] and to increase bone mineral density [6]. Moreover, silicon has been reported to have a positive influence on the synthesis of type I collagen by human osteoblast cells (MG-63 cell line) *in vitro* [7]. Thereby, it is expected that silicon could enhance the hydroxyapatite (HA) bioactivity [8, 9], and silicon-substituted hydroxyapatites (SiHAs) have become a subject of great interest in bone repair. The SiHA structure corresponds to the substitution of phosphate ions (PO_4^{3-}) by silicate ions (SiO_4^{4-}) into the HA crystal structure. Different mechanisms for charge compensation have been suggested [8, 10, 11]. The most cited one was proposed by Gibson et al. with the creation of anionic vacancies at OH^- sites [8, 12]. This mechanism leads to silicon-substituted hydroxyapatites with the general formula $\text{Ca}_{10}(\text{PO}_4)_{6-y}(\text{SiO}_4)_y(\text{OH})_{2-y}(\text{V}_{\text{OH}})_y$, where y represents the molar number of silicate groups introduced into the apatitic structure ($0 \leq y \leq 2$) and V_{OH} stands for vacancies maintaining the charge balance. The incorporation of Si into the HA structure in solid solution, *i.e.* without the formation of other phases, seems to be limited. However, the value and the origin of this limitation are still not known, with for instance the following values: 5 wt% ($\approx 1.7 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [13-15], 4 wt% ($\approx 1.4 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [16, 17], 3.1 wt% ($\approx 1.1 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [18], 2 wt% ($\approx 0.7 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [11, 19], 1.0 wt% ($0.36 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [20] or 0.28 wt% ($0.1 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [21]. Additionally, it has been suggested that the concentration of 0.8 wt% of Si ($\approx 0.28 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) is optimal to induce the development of important bioactivity [22-24]. A value of 2.2 wt% of Si was also reported by Thian et al. [25]. Unfortunately, in spite of extensive studies in recent

years, these results remain heterogeneous, confusing and sometimes misleading. For instance, Hing et al. revealed faster bone apposition and improved adhesion and proliferation of osteoblast-like cells for SiHA compared to stoichiometric HA [23, 26], whereas Palard et al. found no significant difference in the behavior of MG-63 osteoblast-like cells between pure HA and SiHA pellets (three compositions: $y=0.2, 0.4$ and $0.6 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [27]. Recent critical analyses of the published results regarding SiHAs have highlighted the lack of experimental evidence which could explain the real effects of Si substitution on biological activity in a biological environment [28, 29]. In particular, it has been criticized that the physico-chemical characterizations of SiHA bioceramics are not detailed (purity, solubility, rate of incorporation of Si inside the crystal lattice, etc.). Therefore, the available data do not provide sufficient information to establish the origin of the improved biological performance of SiHA: (i) a direct effect of SiHA by Si release, (ii) an indirect effect of SiHA by changes in the physico-chemical properties of HA due to Si substitution (microstructure, superficial chemistry, topography, etc.) or (iii) an effect of second phases (crystalline and/or amorphous). According to Boanini et al., the term “ion-substituted” is quite often used without any experimental proof regarding the incorporation of ions inside the crystal lattice of calcium orthophosphates [28]. The unclear bioactivity of SiHA ceramics could be explained by variations in the phase composition. The first evidence for this was provided by the few accurate analyses available in the literature which show that SiHA powders can contain crystallized [16, 30-35] and amorphous [16, 34, 36-38] impurities. The study by Kanaya et al. is representative of the characterization problems of SiHA samples [38]. Indeed, while the X-ray diffraction patterns show only the characteristic lines of the HA phase (PDF: 09-432), the ^{29}Si MAS NMR spectrum revealed that only 10% of Si was incorporated into the HA lattice; the rest was on the particle surface in the form of polymeric silicate species [38]. An equivalent observation was made by Gasquères et al. [16]. Most studies do not evidently show

the purity of their SiHA samples (powders, pellets or scaffolds) [8, 9, 19, 21-24, 26, 27, 39-58]. They generally provide an imprecise physico-chemical characterization with assumptions based on X-ray diffraction patterns or incomplete infrared band assignment [8, 9, 19, 22, 32, 36, 39, 59-61]. Moreover, infrared vibrations at 692, 840, 890 and 945 cm^{-1} , detected on an SiHA sample containing 1.6 wt% Si (1200°C for 2 h), were attributed without evidence by Gibson et al. to the substitution of SiO_4 for PO_4 into the HA lattice [8, 12]. Unfortunately, this article set the standard for SiHA analysis by infrared spectroscopy and has been widely cited to prove the purity of SiHA powders synthesized using Gibson's method [9, 23, 39, 40, 43, 44, 46, 47, 53, 57] or displaying the same new infrared bands [14, 32, 36, 48, 50, 54, 62].

Several methods are used to prepare Si-substituted hydroxyapatites (SiHAs), such as the sol-gel route [48], resuspension processes [20, 33, 34, 63-66], solid state reactions [10, 67], hydrothermal techniques [17, 68, 69], mechanochemical methods [70], magnetron sputtering [14], pulsed laser deposition [51, 71], electrophoretic deposition [72] and precipitation from aqueous solutions. Aqueous precipitation methods are the most often described and set up in the literature. Two different procedures are used to produce Si-HA from aqueous solutions: (i) the acid-base neutralization [8, 9, 16, 19, 23, 30, 35, 37, 39, 46, 47, 49, 50, 53, 56, 57, 73-75], and (ii) the use of phosphorus and calcium salts [13, 21, 32, 36, 37, 60, 74, 76, 77]. Generally, far less attention has been devoted to the silicon reagent. Two organic compounds are mainly used as a source of silicate ions: tetraethylorthosilicate (TEOS, $\text{Si}(\text{OC}_2\text{H}_5)_4$) and tetraacetoxysilane (TAS, $\text{Si}(\text{COOCH}_3)_4$) which are not miscible in water. Powders synthesized through these methods are poorly crystallized and often contaminated by second phases (e.g. α and β -Tricalcium phosphate, amorphous phase, silicocarnotite [16, 19, 30, 31, 36-38, 49, 59, 60, 63, 64, 67, 74, 76]) or undesired ions like Mg [56], S [77] or Na [78, 79].

In order to correctly describe the physical, chemical and biological properties of SiHAs and to compare them to routinely implanted HA and β -TCP, well-characterized pure SiHAs powders first need to be prepared. Therefore, this work was devoted to the development of a new route to synthesize monophasic SiHA powders with controlled stoichiometry. To this purpose, a solution of soluble silicate was first prepared from TEOS *via* a sol-gel route, and then accurate powder analysis was carried out by means of ICP/AES, X-ray powder diffraction, Rietveld refinement, high resolution electron transmission microscopy (HR-TEM) with energy dispersive spectroscopy (EDS) as well as infrared (FT-IR/ATR) and solid-state NMR spectroscopy. Two pH levels of precipitation were studied, as well as six Si/P molar ratios.

2. Materials and methods

2.1 Powder synthesis

HA and SiHA powders were prepared through an aqueous precipitation method using a fully automated apparatus. A diammonium hydrogen phosphate aqueous solution ($(\text{NH}_4)_2\text{HPO}_4$, 99%, Merck, Germany), and, if applicable, an alkaline silicate solution were added to a calcium nitrate solution ($\text{Ca}(\text{NO}_3)_2 \cdot 4\text{H}_2\text{O}$, 99%, Merck, Germany) using peristaltic pumps. The reaction was performed under an argon flow (4.8, AirLiquide) to prevent any excessive carbonation of precipitates. The pH of the suspension was adjusted by the addition of a 28% ammonia solution (Merck, Germany) by means of a pH stat (Hanna Instruments), and the temperature was controlled and regulated automatically with an external T-probe. The suspension was continuously stirred and refluxed. After complete introduction of the solutions, the suspension was matured for 24 h, and then filtered under vacuum. Finally, the precipitates were dried at 70°C overnight.

The solution of soluble silicates was prepared from tetraethylorthosilicate (TEOS $\geq 99\%$, Aldrich, Germany) *via* a sol-gel route. The original step consisted of the preparation of

a silica gel through the hydrolysis and condensation of this precursor. First, the alkoxide groups (Si-OEt) of TEOS were hydrolyzed to silanol groups (Si-OH). The reaction was catalyzed by a nitric acid aqueous solution ($7.5 \cdot 10^{-3} \text{M}$). This generates a considerable amount of monomers (Si-OH), which aggregate and form a colloidal suspension called the “sol”. This reaction, based on Klein et al. [80], was carried out by maintaining the molar ratio of TEOS/ethanol/acidified water at 1.0/8.5/4.0 and the solution at 25°C in an ambient atmosphere. Second, the condensation of the silanol or alkoxide groups was initiated by increasing the solution pH to a basic level, about pH 8, with a few drops of pure 28% ammonia solution (Merck, Germany). This reaction creates siloxane bridges (Si-O-Si), leading to the formation of a silica gel. The gelation reaction was continued for about 12 h at 25°C . Finally, a solution of soluble silicates was obtained by depolymerization of the silica gel. This was achieved through the nucleophilic attack of siloxane linkages (Si-O) by hydroxide ions in pure 28% ammonia solution ($\text{pH} > 11$). After filtration through a Millipore filtration unit (Magma nylon, $0.8 \mu\text{m}$), the soluble silicate ion concentration of these solutions was measured by means of an ion-exchange chromatography system (DIONEX DX-500) equipped with a SiO_4^{4-} ion exchange column (AS4A) with a UV/Vis detector (410 nm). The soluble silicate ion concentration in these solutions was, on average, $1076 \pm 34 \text{ ppm}$ ($n=14$ solutions). This value is a function of the preparation process (e.g. hydrolysis, condensation and depolymerization reactions). Thereby, the volume of the solutions of soluble silicates was adjusted for each synthesis.

A pure HA powder $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$ was first prepared to be used as a reference material for further SiHA syntheses and analyses. This was obtained at a pH and temperature of precipitation of 9.5 and 50°C , respectively, with a maturation time of 24 h, and a reagent (Ca/P) molar ratio equal to 10/6.

The reagent ratios used to prepare the SiHA powders were calculated by assuming, first, the general formula $\text{Ca}_{10}(\text{PO}_4)_{6-y}(\text{SiO}_4)_y(\text{OH})_{2-y}(\text{VOH})_y$ and, second, a constant molar ratio $\text{Ca}/(\text{P}+\text{Si})$ equal to 10/6. The volume of the calcium and phosphate aqueous solutions was fixed at 500 mL and 250 mL, respectively. Table 1 summarizes the amount (mol) of Ca, P and Si used for each (Si)HA powder prepared with y equal to 0, 0.25, 0.50, 0.75, 1.00, 1.25; designated hereafter as HA, $\text{Si}_{0.25}\text{HA}$, $\text{Si}_{0.50}\text{HA}$, $\text{Si}_{0.75}\text{HA}$, $\text{Si}_{1.00}\text{HA}$ and $\text{Si}_{1.25}\text{HA}$, respectively. Precipitations were achieved at 50°C for 24 h of maturation time, according to the preliminary tests performed on pure HA. Two parameters of precipitation were examined, the pH of precipitation and the stoichiometric number y , *i.e.*, the amount of silicate theoretically incorporated into the apatite structure. Precipitations were conducted either at pH 9.5, previously established for HA synthesis, or at $\text{pH } 10.80 \pm 0.05$. The former was chosen according to phosphate and silicate speciation curves, in order to have HPO_4^{2-} [81] and H_3SiO_4^- ions [82] in solution as the main phosphate and silicate species, respectively. The studied parameters are listed in Table 1.

The as-synthesized powders were heated under air using an alumina crucible. Aliquots of each sample were calcined both at 400°C for 2 h (designated hereafter as “raw powders”), in order to remove synthesis residues, and at 1000°C for 15 h under air according to ISO norm 13779-3 in order to characterize powders with a well-defined structure. The heating and cooling rate was fixed at 4°C min⁻¹.

2.2 Powder characterization

2.2.1 X-ray powder diffraction and Rietveld refinement

Crystalline phases were identified by means of a Siemens D5000 $\theta/2\theta$ X-ray diffractometer (XRD) using $\text{CuK}\alpha$ radiation and operating at 40 kV and 20 mA. XRD patterns were first collected over the 2θ range of 10-60° at a step size of 0.03° and counting time of 4 s per step in order to determine the phase composition. Crystalline phases detected in the patterns were

identified by comparison to standard patterns from the ICDD-PDF (International Center for Diffraction Data-Powder Diffraction Files). In addition, high resolution XRD scans were obtained on calcined powders from 10° to 120° in 0.02° steps with a counting time of 10.5 s per step. These patterns were used to calculate the lattice parameters and the crystalline size by full pattern matching. In this mode, the positions of the diffraction peaks and the systematic extinctions are calculated from the cell parameters and the space group. The intensities of the lines are adjusted by the refinement program and not calculated from the atomic positions. The refinements were performed using the space group of the HA structure P63/m (PDF 09-432) by means of the Topas software (Bruker, Germany). The initial cell parameters were taken as $a = 9.42\text{\AA}$ and $c = 6.88\text{\AA}$.

The evolution of the crystallinity of the samples after calcination at 1000°C for 15 h was evaluated by means of the full width at half maximum (FWHM) of the (211) peak at $2\theta=31.8^\circ$, as it had the highest intensity and minimal overlap with neighboring peaks.

2.2.2 Infrared spectroscopy

Fourier transform infrared (FT-IR) measurements were carried out with the use of a MIR TF VERTEX 70 Spectrometer by means of the ATR system. The spectra were recorded over the range of $450\text{--}4000\text{ cm}^{-1}$ with a resolution of 2 cm^{-1} . Spectra were obtained by signal averaging 32 successive scans. Every measurement was at least duplicated on two independent powder samples crushed by hand, with an agate pestle and mortar, and deposited on the ATR system. Spectra were normalized with respect to the ν_4 band of the phosphate group at about 602 cm^{-1} , according to a classical procedure [83, 84].

2.2.3 NMR spectroscopy

NMR spectra were recorded on a Bruker AVANCE 300 spectrometer: $B_0 = 7.05\text{ T}$, $\nu_0(^1\text{H}) = 300.13\text{ MHz}$, $\nu_0(^{31}\text{P}) = 121.49\text{ MHz}$, $\nu_0(^{29}\text{Si}) = 59.62\text{ MHz}$, using a CP-MAS Bruker probe with 4 mm rotors spinning at 14 kHz for ^1H and ^{31}P and with 7 mm rotors spinning at 5

kHz for ^{29}Si . Chemical shifts are referenced to TMS for ^1H and ^{29}Si and 85% aqueous H_3PO_4 for ^{31}P . Single pulse and CP (cross-polarization) MAS experiments have been used to study these materials. CP MAS relies on the heteronuclear dipolar interaction between an abundant spin X (^1H here) and a low abundant nuclei Y (^{31}P and ^{29}Si here). It allows the study of local molecular motion. The NMR parameters are summarized in Table 2.

2.2.4 Electron microscopy (HR-TEM, SAED and EDX)

High resolution transmission electron microscopy (HR-TEM) was conducted on calcined powders ($1000^\circ\text{C}/15\text{ h}$) using a JEOL 2010 F Microscope at a voltage of 200 kV. Samples were prepared by dispersing the powders in ethanol. After sonication at 40 W for 5 min, a small drop of the suspension was placed onto copper mesh grids coated with a holey carbon film. Finally, a thin coating of gold (10 nm in thickness) was sputtered on half of the grid. Gold was then distributed as crystallized nano-domains which were used as a reference in the selected area electron diffraction (SAED) patterns to calculate as precisely as possible the lattice parameters. The SAED patterns obtained from regions with or without gold on the HA part were the same.

2.2.5 Elemental analysis

The silicon, phosphorous and calcium content in powders was determined by inductively coupled plasma atomic emission spectrometry (ICP/AES) (HORIBA Spectrometer, Jobin-Yvon, Activa model). Powder samples were dissolved in a nitric acid solution (0.5 M). Solutions were prepared (e.g. powder mass, dilution) in order to limit the measurement uncertainty as well as to determine the concentrations of Ca, P and Si within the highest sensitivity range of the ICP/AES device (around 30 ppm). Lastly, the carbon content in the powders was determined using an elemental analyzer with an infrared detector (LECO CS-444 carbon and sulfur analyzer).

The stoichiometric number y was determined by means of Eq. 4, assuming that powders containing $0 \leq \text{wt\%Si} \leq 2.81$ (or $0 \leq y \leq 1.00$) are pure monophasic SiHAs $\text{Ca}_{10}(\text{PO}_4)_{6-y}(\text{SiO}_4)_y(\text{OH})_{2-y}(\text{VOH})_y$, without any second crystalline or amorphous phase.

$$\% \text{ wt Si} = (m_{\text{Si}} 100 / m_{\text{Si}y\text{HA}}) = (C_{m_{\text{Si}}} V_{\text{sol}} 100) / (m_{\text{Si}y\text{HA}}) \quad (1)$$

$$n_{\text{Si}} = (\% \text{ wtSi } m_{\text{Si}y\text{HA}}) / (M_{\text{Si}} 100) \quad (2)$$

$$M_{\text{Si}y\text{HA}} = M_{\text{HA}} - (19.895 y_{\text{Si}}) \quad (3)$$

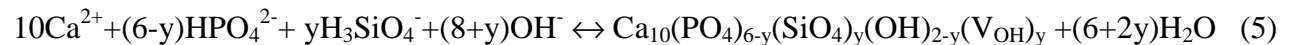
$$y_{\text{Si}} = (n_{\text{Si}} M_{\text{Si}y\text{HA}}) / (m_{\text{Si}y\text{HA}}) = (\% \text{ wtSi } M_{\text{HA}}) / (100 M_{\text{Si}} + 19.985 \% \text{ wt Si}) \quad (4)$$

where $\% \text{ wt Si}$ is the mass percentage of Si in the powder, $C_{m_{\text{Si}}}$ is the mass concentration of Si in the analyzed solution by ICP/AES (ppm or mg L^{-1}), V_{sol} is the volume of the analyzed solution (L), $m_{\text{Si}y\text{HA}}$ is the mass of the powder dissolved in the former solution (mg), and $M_{\text{Si}y\text{HA}}$, M_{HA} and M_{Si} are the molar masses of SiyHA, HA and Si, respectively (g mol^{-1}).

3. Results and discussion

3.1 Influence of pH on the SiHA phase composition

$\text{Si}_{0.50}\text{HA}$ powders were synthesized at 50°C with pH values equal to 9.50 ($\text{Si}_{0.50}\text{HA}$ -9.5) and 10.80 ($\text{Si}_{0.50}\text{HA}$ -10.8). Fig. 1 shows the XRD diffractograms of powders calcined at 1000°C for 15 h. The pattern of the $\text{Si}_{0.50}\text{HA}$ -9.5 sample presents two different crystalline phases matching the ICDD standard for hydroxyapatite (HA, PDF 9-432) and α -tricalcium phosphate (α -TCP, PDF 9-348). The $\text{Si}_{0.50}\text{HA}$ -10.8 diffractogram displays only the characteristic diffraction lines of HA. This result indicates that the final composition of the powders is a function of silicate ion speciation. H_3SiO_4^- or more basic forms of silicate ions have to be maintained during the synthesis to obtain a thermally stable SiHA phase, *i.e.* a monophasic powder after heat treatment at $1000^\circ\text{C}/15$ h. Therefore, herein, the following results are presented for powders prepared at pH 10.8. Under these synthesis conditions, the general reaction of precipitation can be written as follows:



To our knowledge, this is the first time that a true precipitation reaction has been given for SiHA.

3.2 Influence of the Si content (y_{Si})

3.2.1 X-ray diffraction analysis

Fig. 2 shows the diffraction patterns of HA and Si_yHA ($y_{\text{Si}} = 0.25, 0.50, 0.75, 1.00$ and 1.25 mol) raw powders. Each pattern matches well with the standard pattern of HA (PDF 9-432). No other phase was detected. The samples exhibit broad diffraction lines which indicate very small crystallites and/or low crystallinity. More, the FWHM increased with silicon content. The diffractograms of heat treated powders ($1000^\circ\text{C}/15$ h) are displayed in Fig. 3. They present no secondary phase besides hydroxyapatite for a silicon content up to $y_{\text{Si}} = 1.00$. On the other hand, HA (PDF 9-432) and α -TCP (PDF 9-348) were detected in the pattern of $\text{Si}_{1.25}\text{HA}$ calcined at 1000°C for 15 h. Moreover, as observed for the raw powders, the crystallinity of Si_yHA calcined powders with $1 \geq y \geq 0$ decreased with an increase in the silicate content. Indeed, the higher the Si content, the higher the FWHM of the diffraction line. For instance, the FWHM of the diffraction line at 31.8° (2θ) increased as follow: 0.070 (HA) < 0.096 ($\text{Si}_{0.25}\text{HA}$) < 0.160 ($\text{Si}_{0.50}\text{HA}$) < 0.164 ($\text{Si}_{0.75}\text{HA}$) < 0.170 ($\text{Si}_{1.00}\text{HA}$). This is due to both direct (decrease in the crystallinity) and indirect (decrease in the crystallite size) effects of Si, but the individual contributions of these effects cannot be evaluated by X-ray diffraction.

The XRD patterns indicate that whatever the amount of silicon ranging between $0 \leq \text{wt\%Si} \leq 3.51$ (or $0 \leq y \leq 1.25$), the crystalline phase of the precipitates is a hydroxyapatite (PDF 09-432). Thereby, silicon can be incorporated in the apatitic structure, or in an amorphous phase or in both phases. However, only precipitates containing up to 2.81 wt%Si (or $y = 1.00$) are thermally stable at 1000°C for 15 h.

3.2.2 Lattice parameter refinement

Refinement was performed on monophased heat-treated powders ($0 \leq y \leq 1.00$). The results, displayed in Table 3, reveal changes in the apatitic structure parameters. The Si substitution causes *c*-axis and unit cell volume expansion as well as a reduction in the mean crystallite size. The same observation was reported in other studies [10, 17, 32, 70, 85]. On the other hand, and in contrast to the linear increase of the lattice parameter *c* with an increasing amount of Si, the *a* lattice parameter fluctuates at random between 9.416 Å and 9.428 Å. These results highlight that all or part of the silicon is incorporated into the apatitic structure.

3.2.3 Elemental analysis

The experimental Ca/(P+Si) molar ratios of the final calcined powders are presented in Table 1. Values are in accordance with the expected ones (1.67) for all compositions, considering experimental error. Moreover, the calcined powders were not carbonated since the carbon content by weight was equal to 0.03, 0.07, 0.05, 0.05 and 0.05 wt% (± 0.02 wt%) for HA, Si_{0.25}HA, Si_{0.50}HA, Si_{0.75}HA and Si_{1.00}HA, respectively.

The results, presented in Table 1, show that the chemical formulas of SiHA calculated first by the measured silicon contents, then by the theoretical formula $\text{Ca}_{10}(\text{PO}_4)_6 \cdot y(\text{SiO}_4)_y(\text{OH})_{2-y}(\text{V}_{\text{OH}})_y$ and finally using Eq. 4 are in a good agreement with the nominal ones.

3.2.4 Electron microscopy

A low magnification bright-field image of heat-treated Si_{1.00}HA particles is shown in Fig. 4a. SiHA powders are composed of round particles, smaller than 100 nm in diameter for Si_{1.00}HA, whereas the HA powder shows bigger acicular crystals [86]. At higher magnification, grains do not present any dislocation or disorder within the central region. Similarly, high-resolution lattice images of the grain surface do not show any amorphous or disordered layer (see Fig. 4b). A selected area electron diffraction (SAED) pattern obtained on the same grain is displayed in Fig. 5a. SAED patterns show a diffraction pattern with well-defined spots regardless of the selected area. This indicates the high crystallinity of the heat-

treated SiHA powders and the homogeneity of the crystals. Second, a very good agreement appears between the SAED patterns and the PDF card 09-432 of HA as identified by X-ray diffraction. Moreover, no halo ring was observed, confirming the absence of the amorphous phase. Fig. 5b shows a SAED pattern for the [010] zone axis. Two other SAED patterns were obtained for the [1-10] zone axis. Indexation of these patterns allows for calculating the c/a ratio by means of the interval between two spots. Thus, for instance, according to the hexagonal crystallographic structure identified by X-ray diffraction and the distance D_1 and D_2 between two spots along the [h00] and [001] directions ([010] zone axis, Fig. 5b), respectively, the c/a ratio was calculated as follows:

$$(c/a)^2 = \frac{3}{4} (D_1/D_2)^2 \quad (6)$$

The results are the average of about ten intervals per pattern. A c/a ratio of 0.730 ± 0.005 was determined. Moreover, other experimental patterns for different zone axes (not shown here) were obtained and compared to theoretical electron diffraction patterns calculated by means of the Java Electron Microscopy Simulation (JEMS) software [87]. The results indicate that the experimental and simulated patterns are perfectly superimposed for $0.734 \geq c/a \geq 0.729$. Additionally, the c/a ratio value from PDF 09-432 (0.7309) is included in this range.

3.2.5. Solid-state NMR analysis

3.2.5.1. ^{31}P MAS NMR

The ^{31}P MAS NMR spectra of HA, $\text{Si}_{0.50}\text{HA}$ and $\text{Si}_{1.00}\text{HA}$ calcined at 1000°C for 15 h are shown in Fig. 6a. The spectra present a main narrow peak which corresponds to the single P site of hydroxyapatite [88], and whose position shifts to higher frequencies with increasing silicon content: 2.8 ppm for HA, 3.0 ppm for $\text{Si}_{0.50}\text{HA}$, and 3.1 ppm for $\text{Si}_{1.00}\text{HA}$. Likewise, the FWHM broadens: $166 \text{ Hz} < 188 \text{ Hz} < 233 \text{ Hz}$ for raw HA, $\text{Si}_{0.50}\text{HA}$ and $\text{Si}_{1.00}\text{HA}$, respectively (figure not included), and $55 \text{ Hz} < 132 \text{ Hz} < 233 \text{ Hz}$ for calcined HA, $\text{Si}_{0.50}\text{HA}$

and Si_{1.00}HA, respectively (Fig. 6a). The chemical shift and peak broadening indicate that the SiHA structure is different from a perfect hydroxyapatite short-range structure. The increasing line width suggests an increase in local disorder around those phosphate groups where Si is incorporated in the HA structure. Besides the 2.8 ppm peak, two additional weak broad peaks at 4.6 and 5.8 ppm were detected in the ³¹P spectra. The peak at 4.6 ppm was only revealed in the ¹H → ³¹P CP MAS spectrum (Fig. 7b). HA powder did not present the 4.6 ppm signal (Fig. 7a). According to Hartmann et al. [89], the ³¹P MAS peak at 5.8 ppm corresponds to PO₄ tetrahedra in a proton-free region of a hydroxyapatite channel structure containing OH vacancies (*i.e.* along the crystallographic *c*-axis). These proton-free regions, observed in oxyhydroxyapatite Ca₁₀(PO₄)₆(OH)_{2-2x}(O)_x(V_{OH})_x (OHA), must exist in silicon-substituted hydroxyapatite Ca₁₀(PO₄)_{6-y}(SiO₄)_y(OH)_{2-y}(V_{OH})_y (SiHA), or silicon-substituted oxyhydroxyapatite Ca₁₀(PO₄)_{6-y}(SiO₄)_y(OH)_{2-y-2x}O_x(V_{OH})_{x+y} (SiOHA). The assignment of the peak at 4.6 ppm, that seems related to the incorporation of Si in the apatite lattice, will be discussed later on (section 3.2.5.3).

3.2.5.2. ¹H MAS NMR

The ¹H MAS NMR spectra of pure HA, Si_{0.50}HA and Si_{1.00}HA powders calcined at 1000°C for 15 h are shown in Fig. 6b. Two signals were observed, one sharp at 0 ppm and one broader at about 5.2 ppm. The former (0 ppm) is characteristic of OH groups in crystalline HA [89]. Moreover, and similarly to the ³¹P signal at 2.8 ppm, the greater the Si content in the apatitic structure of the calcined powders, the broader the FWHM of the signal at 0 ppm (FWHM = 108 Hz for HA, 191 Hz for Si_{0.5}HA and 228 Hz for Si_{1.00}HA). This suggests a change in the environment around the hydroxyl groups, highlighting the modification of O-H bond distances due to Si. As postulated by Gomes et al., this concomitant broadening of the ³¹P and ¹H resonances with Si content confirms the incorporation of Si atoms into the apatite lattice [30]. The signal at 5.2 ppm was attributed by Hartmann et al. to OH⁻ positions missing

only one neighboring ion in OHA channels [89]. This type of OH⁻ group along the channels of the apatite structure leads to the formation of “proton pairs” stabilized by a hydrogen bond. The intensity of this proton position is higher in SiHA samples than in HA, but does not seem to be an exclusive function of the Si content (see Fig. 6b). Therefore, ¹H MAS NMR indicates the presence of two types of OH⁻ groups along the channels of the apatite structure: an unchanged proton line position with continuous OH⁻ groups (0 ppm) and OH⁻ pairs surrounded by vacancies (5.2 ppm).

3.2.5.3. ¹H-³¹P HETCOR CP MAS

To confirm that the entire proton position is located in the apatite channel structure, two-dimensional ¹H-³¹P HETCOR CP MAS experiments were performed on raw and calcined powders. Fig. 8 presents ¹H-³¹P HETCOR CP MAS spectra recorded on raw Si_{1.00}HA (Fig. 8a) and calcined Si_{0.50}HA (Fig. 8b) powders. The spectra show two main 2D correlation peaks on both raw and calcined powders. The same peaks were observed for Si_{0.25}HA, Si_{0.50}HA and Si_{1.00}HA (HETCOR CP MAS results for calcined Si_{0.25}HA and Si_{1.00}HA not included). The stronger one (peak A, Fig. 8b), characteristic of an ideal HA structure, is due to the dipolar interaction between the P sites ($\delta(^{31}\text{P}) = 2.8$ ppm) and the OH sites ($\delta(^1\text{H}) = 0$ ppm). It corresponds to an undisturbed hydroxyapatite short-range structure [89]. The second one (peak B, Fig. 8b) appears between the ³¹P signal at 4.6 ppm and the ¹H signal at 5.2 ppm. Its intensity increases with heat treatment (Fig. 8) and the Si content (data not included). This correlation is not observed for the HA sample (data not included). Moreover, a low extent of peak B is observed with the main ³¹P peak at 2.8 ppm (peak C, Fig. 8b). The intensity of this 2D correlation peak becomes stronger with Si content as well. More generally, the higher the amount of Si incorporated into the SiHA structure, the stronger the dispersion of the main correlation between A and B along the ³¹P axis. Finally, as expected, the HETCOR spectra show no correlation peak of the ³¹P line at 5.8 ppm, confirming that it corresponds to a

proton-free phosphate position. To conclude, first the broadening of peak A indicates an increase in the distribution of P-H bond distances when silicate is incorporated into the HA structure, corresponding to the loss of local ordering in the phosphate environment. Second, peaks B and C correspond to two distinct P sites in the vicinity of isolated pairs of protons (OH^- pairs) present in the channel structure of silicon-substituted oxyhydroxyapatite $\text{Ca}_{10}(\text{PO}_4)_{6-y}(\text{SiO}_4)_y(\text{OH})_{2-y-2x}\text{O}_x(\text{VOH})_{y+x}$ (SiOHA): (i) peak B represents a very strongly distorted hydroxyapatite short-range structure and (ii) peak C represents a less distorted one. Peak B is clearly related to SiO_4 substitution and proves once again that charge compensation implies OH vacancies along the channels, leading to the formation of OH^- pairs in the vicinity of the substituted PO_4 tetrahedra. Peak C can be due to SiO_4 substitution as well as dehydration of SiHA, both leading to the formation of OH vacancies in SiOHA.

3.2.5.4. ^{29}Si MAS NMR

The ^{29}Si MAS NMR spectra of $\text{Si}_{1.00}\text{HA}$ powders, raw and calcined, are shown in Fig. 9. The raw powders present two resonances: one sharp at about -72 ppm that is clearly attributed to SiO_4^{4-} (Q^0) in the apatitic structure [90], and a broad peak at about -100/-110 ppm which corresponds to Q^3/Q^4 silicon species [16]. The results confirm that the main part of the silicate is incorporated into the HA lattice during precipitation, according to the main reaction Eq. 1. The rest of the silicates are adsorbed at the crystallite surface, as observed for phosphates during the precipitation of apatitic calcium phosphates [91, 92]. After calcination, the broad peak at -100/-110 ppm disappears without the detection of new signals, similar to those reported in the literature (Si-TCP or $\alpha\text{-Ca}_3\text{Si}_3\text{O}_9$) [16, 30, 38]. The same results were obtained for the $\text{Si}_{0.25}\text{HA}$ and $\text{Si}_{0.50}\text{HA}$ samples (data not included).

3.2.6. FT-IR analysis

3.2.6.1 As-synthesized samples

The IR spectra of the raw HA and SiHA powders with a silicon content up to $y_{\text{Si}} = 1.25$ mol (figure not included) present strong similarities and exhibit intense bands characteristic of hydroxyapatite. They correspond to the four vibrational modes of phosphate groups (ν_1 , ν_2 , ν_3 , and ν_4), and the stretching (ν_s) and librational (ν_L) modes of the hydroxide groups [81, 92-94]. The intensity of the latter, at 630 cm^{-1} (ν_L) and 3570 cm^{-1} (ν_s), clearly decreased with the amount of silicon. These results confirm that the as-synthesized precipitates exhibit the hydroxyapatite phase, regardless of the amount of silicon ranging between $0 \leq \text{wt\%Si} \leq 3.51$ (or $0 \leq y \leq 1.25$), as observed on the diffractograms (Fig. 2). A more accurate description of the infrared spectra of the as-synthesized SiHA powders is available in a complementary article [95].

3.2.6.2 Calcined samples – general observations

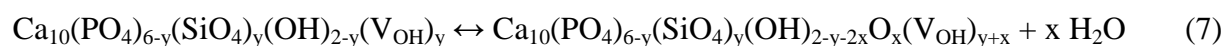
Fig. 10 compares the infrared spectra of heat-treated HA and SiHA powders ($1000^\circ\text{C}/15 \text{ h}$). The HA and Si_yHA with $0 \leq y \leq 1.0$ powders mainly present bands characteristic of hydroxyapatite with the ν_1 (962 cm^{-1}), ν_2 (473 cm^{-1}), ν_3 (1021 and 1085 cm^{-1}) and ν_4 (562 and 600 cm^{-1}) modes of PO_4^{3-} , as well as the stretching (ν_s : 3572 cm^{-1}) and librational (ν_L : 629 cm^{-1}) modes of hydroxide groups [81, 92, 94]. A shoulder at 947 cm^{-1} was also observed for HA and SiHA powders. The relative intensity of this shoulder was slightly higher for SiHA than for HA, but did not seem to be a function of the amount of Si. Besides the low hydroxyapatite vibrations, the spectrum of the $\text{Si}_{1.25}\text{HA}$ powder presents mainly the characteristic bands of α -TCP and traces of β -tricalcium phosphates (β -TCP): the weak band at 495 cm^{-1} ascribed to the O-P-O ν_2 vibrational mode of β -TCP, the bands due to the splitting of the ν_4 mode at 567 cm^{-1} in α -TCP (551 , 560 , 580 , 595 and 611 cm^{-1}), the bands at 945 and 955 cm^{-1} assigned to the degenerated symmetric P-O stretching vibration of the phosphate ions (ν_1) in β - and α -TCP, respectively, and the bands corresponding to the strong asymmetric P-O stretching mode (ν_3) for β -TCP (988 , 1025 cm^{-1}) and α -TCP (988 , 1013 , 1025 , 1031 and 1055 cm^{-1}) [52,

96]. This result is complementary to the X-ray diffraction pattern (Fig. 3) and indicates that the $\text{Si}_{1.25}\text{HA}$ apatitic precipitate decomposes during heat treatment with the formation of TCP and amorphous silica species.

3.2.6.3. Calcined samples – accurate IR band assignment of the pure SiHA phase

As opposed to HA, the FT-IR spectra of the calcined Si_yHA powders, with $0 \leq y \leq 0.75$, exhibit nine new bands or shoulders (sh) at 491 (sh), 504, 528, 750, 840, 893, 930 (sh), 985 (sh) and 1002 (sh) cm^{-1} . The intensity of these new vibrations increased with the amount of Si, except for the weak band at 840 cm^{-1} and the shoulder at 930 cm^{-1} which remained relatively constant. Conversely, the intensity of the absorption bands attributed to the four vibrational modes of PO_4^{3-} and both modes of OH^- in hydroxyapatite decreased as the amount of Si increased in the range $0 \leq y \leq 1.00$ (e.g. $\nu_s \text{ OH}^- : 0.49 (\text{HA}) > 0.39 (\text{Si}_{0.25}\text{HA}) > 0.35 (\text{Si}_{0.50}\text{HA}) > 0.12 (\text{Si}_{0.75}\text{HA}) > 0.07 (\text{Si}_{1.00}\text{HA})$). More precisely, the ν_L mode decreased to the detection limit for $y = 1$, while the stretching the OH^- band decreased and broadened. In fact, two new vibrations at 3565 and 3552 cm^{-1} , close to the main one at 3572 cm^{-1} , were detected (Fig. 10). This confirms the mechanism of charge compensation with the creation of OH^- vacancies, and highlights the new environment and distribution of OH^- ions along the channels of the SiHA structure [93, 97] and, more importantly, the formation of low hydrogen bonding between closed O^{2-} and OH^- ions (H-bonds cause a shift of 20 cm^{-1} to the low wavenumber of the main band at 3572 cm^{-1} [98]). The FT-IR spectrum of $\text{Si}_{1.0}\text{HA}$ displays the same eight new bands as those detected on $\text{Si}_{0.25}\text{HA}$, $\text{Si}_{0.50}\text{HA}$ and $\text{Si}_{0.75}\text{HA}$. However, their relative intensity decreased significantly, reaching the detection limit for the band at 750 cm^{-1} and with a complete disappearance of the bands at 491, 504, and 528 cm^{-1} . Additionally, seven new vibrations appeared at 500, 515, 535, 683, 798 and 873 cm^{-1} . They were accompanied by an intensification of the shoulder at 947 cm^{-1} . The bands at 683, 798 and 870 cm^{-1} were also detected in spectrum of $\text{Si}_{1.25}\text{HA}$ calcined powder. According to these results

and an accurate review of the bibliography, summarized in Table 4, it is clear that the nine vibrations at 493, 504, 528, 750, 840, 893, 930, 985 and 1002 cm⁻¹ are related to the incorporation of Si into the hydroxyapatite structure. The changes detected in the sample Si_{1.0}HA were due to the start of decomposition of the SiHA phase, emphasized by a decrease in the nine characteristic bands and the formation of an amorphous silica phase which presents vibrations at 500, 515, 535, 683, 798 and 873 cm⁻¹. Silica was not detected by NMR due to the low amount of ²⁹Si in the samples (high detection limit). The shoulder at 947 cm⁻¹ could be attributed to β-TCP, which exhibits a symmetric P-O stretching mode ν₁ at 945 cm⁻¹ [96]. However, this assumption is not convincing since other bands assigned to β-TCP are absent. In fact, this shoulder is a contribution of the Si-O in plane stretching vibrations in Si-OH and Si-O⁻ on the surface of the grains, and the symmetric stretching (ν₁) vibration of orthophosphate groups in the neighborhood of OH vacancies along the channels. The former, reported at 950 cm⁻¹ (see Table 4), shifted toward lower frequencies due to hydrogen bonding between surface groups, thus creating the component at 930 cm⁻¹. The band at 950 cm⁻¹ is commonly observed for oxy-hydroxyapatite Ca₁₀(PO₄)₆(OH)_{2-2x}O_x(V_{OH})_x, [93, 99-102]. Therefore, in the context of this study, OH⁻ vacancies (V_{OH}) are due first to the incorporation of SiO₄ into the HA structure, and second to the partial dehydration of SiHA to SiOHA as follows:



3.2.6.4. Calcined samples – OH vacancies and the limit of incorporation of Si in HA

The amount of hydroxide (%OH) in the silicon-substituted hydroxyapatite structure is reported versus the amount of silicon (mol mol_{SiHA}⁻¹) in Fig. 11. The theoretical values of OH were plotted by considering the formula Ca₁₀(PO₄)_{6-y}(SiO₄)_y(OH)_{2-y}(V_{OH})_y (*i.e.* %OH = 100 - 50 y). The experimental values were determined at room temperature on the calcined samples (1000°C/15 h) by means of the integrated area of the ν_L and ν_S OH bands. The average of the

495 integrated areas obtained for HA ($y=0$) was assumed to be representative of the full
 496 occupancy of the OH position within the channels (100% OH). The amount of OH vacancies
 497 (V_{OH}) determined experimentally was always higher than the theoretical one with respect to
 498 the chemical formula $Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y}(V_{OH})_y$. In other words, the dehydration of
 499 the calcined powders was greater than expected, and a higher Si doping level led to a greater
 500 difference. Thus, the incorporation of Si into the hydroxyapatite structure generates OH
 501 vacancies first to maintain the charge balance ($Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y}(V_{OH})_y$) and second
 502 from another phenomena, which is an increasing function of the amount of Si. A possible
 503 explanation is an increase of the mobility of OH ions along the channel axis (local disorder)
 504 and their subsequent rate of diffusion and debonding from the HA lattice [103]. HA
 505 decomposition is a dynamic process, mainly controlled by the degree of dehydration [104-
 506 106]. In fact, the thermal stability of hydroxyapatite was found to depend on the fraction of
 507 V_{OH} and O^{2-} ions in the channels. Several “critical values” of V_{OH} in OHA $Ca_{10}(PO_4)_6(OH)_{2-}$
 508 $_{2x}O_x(V_{OH})_x$ have been reported beyond which the apatite channel structure is destroyed: $x \leq$
 509 0.80 [103], $x \leq 0.75$ [107], $x \leq 0.50$ [89]. However, the most probable limit comes from work
 510 of Heughebaert and Montel on the crystallization of calcium phosphates during precipitation
 511 [108, 109]. They determined that the apatitic structure appears only when at least 25% of the
 512 OH^- positions along the channels are really occupied. In other words, the apatitic structure
 513 appears when $V_{OH} < 1.5$. Therefore, the theoretical maximum limit of incorporation of Si into
 514 a hexagonal apatitic structure is $y < 1.5$ as regards the formula $Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-}$
 515 $_y(V_{OH})_y$. However, due to the dehydration reaction (Eq. 7), this limit is a function of the
 516 temperature and the atmosphere of heat treatment. This assumption can explain why the
 517 $Si_{1.0}HA$ and $Si_{1.25}HA$ powders, which showed an apatitic structure after calcination at $400^\circ C$
 518 for 2 h, were not thermically stable at $1000^\circ C$ for 15 h in contrast to $SiHA$ with a silicon
 519 content ranging between $0 \leq y \leq 0.75$. Control of the degree of hydroxylation, *i.e.* the partial

steam pressure p_{H_2O} , is necessary to control the thermal stability of the SiHA phase. This assumption is confirmed by the infrared spectra obtained from the $Si_{1.0}HA$ sample heat treated at 1000°C for 15 h under different partial pressures of steam, p_{H_2O} , in mbar (Fig. 12); a higher p_{H_2O} led to a more stable silicon-substituted apatite phase. Thus, the $Si_{1.0}HA$ powder, after calcination under high steam pressure ($p_{H_2O} = 200$ mbar), presented only the characteristic bands of SiHA with traces of amorphous silica at the IR spectroscopy detection limit ($\approx 0.1\text{wt}\%$), whereas the same sample heat-treated under dry argon gas ($p_{H_2O} = 0$ mbar) contained amorphous silica species as well as TCP (α and β). Moreover, the vibrations related to Si-O in SiHA (750 and 890 cm^{-1}) as well as the vibrational modes ν_3 and ν_4 of the phosphate groups in HA decreased with a decrease in p_{H_2O} . Conversely, the vibrations due to amorphous silica species, at 683 , 798 and 873 cm^{-1} , and TCP (e.g. 731 , 942 , 997 and 1137 cm^{-1}) increases with a decrease in p_{H_2O} .

These results confirm that the formation of amorphous silica and the decomposition of the SiHA phase are correlated. More precisely, the detection of amorphous silica indicates the start of decomposition, which is followed by the formation of TCP (α and β).

Finally, Trombe and Montel reported the variation of a from 9.421 \AA to 9.402 \AA , without a significant variation in the c lattice parameter, when HA transforms into OHA, $Ca_{10}(PO_4)_6(OH)_{0.5}O_{0.75}(V_{OH})_{0.75}$ [102]. Thus, SiHA dehydration can explain the random fluctuations in the a lattice parameter observed in this work and in the literature [30].

4. Conclusion

This paper presents a new route to synthesize monophasic silicon-containing hydroxyapatites $Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y}(V_{OH})_y$ (SiHAs) with controlled stoichiometry. The combination of solid state nuclear magnetic resonance (NMR) and IR spectroscopy (IR) demonstrated that silicate substitution for phosphate creates OH vacancies along the channels. Moreover, Si substitution increases the local disorder and the mobility of OH ions along these channels and

their subsequent rate of diffusion and debonding from the HA lattice. The control of the degree of hydroxylation of the SiHA phases, *i.e.* their thermal stability, can be carried out by means of the partial steam pressure, p_{H_2O} . Additionally, an exhaustive description of the infrared bands related to the incorporation of silicate groups into the HA structure was established. It allowed us to determine that the literature has incorrectly attributed some infrared bands to silicate groups in the apatite structure. These bands, e.g. 683, 798 and 873 cm^{-1} , due in fact to amorphous silica phases, raise questions regarding the phase purity of the great majority of biologically evaluated SiHA bioceramics.

Acknowledgments

The authors wish to thank the “Region Rhône-Alpes” for the financial support provided for this work.

References

- [1] Carlisle EM. Silicon: A Possible Factor in Bone Calcification. *Science* 1970;167:279-80.
- [2] Carlisle EM. In vivo requirement for silicon in articular cartilage and connective tissue formation in the chick. *The journal of nutrition* 1976;106:478-84.
- [3] Nielsen FH, Poellot R. Dietary silicon affect bone turnover differently in ovariectomized and sham-operated growing rats. *The journal of the trace elements in experimental medicine* 2004;17:137-49.
- [4] Schwarz K, Milne D. Growth promoting effects of silicon in rats. *Nature* 1972;239 333-4.
- [5] Damen JJM, M. TCJ. Silica-induced Precipitation of Calcium Phosphate in the Presence of Inhibitors of Hydroxyapatite Formation. *Journal of dental Research* 1992;71:453-7.
- [6] Jugdaohsingh R. Silicon and bone health. *The Journal of Nutrition Health and Aging* 2007;11:99-110.
- [7] Reffitt DM, Ogston N, Jugdaohsingh R, Cheung HFJ, Evans BAJ, Thompson RPH, et al. Orthosilicic acid stimulates collagen type 1 synthesis and osteoblastic differentiation in human osteoblast-like cells in vitro. *Bone* 2003;32:127-35.
- [8] Gibson IR, Best SM, Bonfield W. Chemical characterization of silicon-substituted hydroxyapatite. *J Biom Mat Res* 1999;44:422-8.
- [9] Patel N, Best SM, Bonfield W, Gibson IR, Hing KA, Damien E, et al. A comparative study on the in vivo behavior of hydroxyapatite and silicon substituted hydroxyapatite granules. *J MatSci: Materials in Medicine* 2002;13:1199-206.
- [10] Arcos D, Rodríguez-Carvajal J, Vallet-Regí M. The effect of the silicon incorporation on the hydroxylapatite structure. A neutron diffraction study. *Solid State Sciences* 2004;6:987-94.
- [11] Astala R, Calderin L, Yin X, Stott MJ. Ab Initio Simulation of Si-Doped Hydroxyapatite. *Chem Mat* 2006;18:413-22.
- [12] Gibson IR, Huang J, Best SM, Bonfield W. Enhanced *in vitro* cell activity and surface apatite layer formation on novel silicon-substituted hydroxyapatites. *Bioceramics* 1999;12:191-4.
- [13] Best S, Bonfield W, R. Gi, Jha LJ, Da Silva Santos JD. Silicon-substituted apatites and process for the preparation thereof. United States Patent, US 6,312,468 B1
Great Britain, London1998.
- [14] Thian ES, Huang J, Vickers ME, Best SM, Barber ZH, Bonfield W. Silicon-substituted hydroxyapatite (SiHA): A novel calcium phosphate coating for biomedical applications. *Journal of Materials science* 2006;41:709-17.
- [15] Vallet-Regí M, Arcos D. Silicon substituted hydroxyapatites. A method to upgrade calcium phosphate based implants. *Journal of Materials chemistry* 2005;15.
- [16] Gasquères G, Bonhomme C, Maquet J, Babonneau F, Hayakawa S, Kanaya T, et al. Revisiting silicate substituted hydroxyapatite by solid-state NMR. *Magn Reson Chem* 2008;46:342-6.
- [17] Tang XL, Xiao XF, Liu RF. Structural characterization of silicon-substituted hydroxyapatite synthesized by a hydrothermal method. *Materials Letters* 2005;59:3841-6.

- [18] Gomes S, Nedelec J-M, Jallot E, Sheptyakov D, Renaudin G. Silicon location in silicate-substituted calcium phosphate ceramics determined by neutron diffraction. *Crystal growth and design* 2011;11:4017-26.
- [19] Kim SR, Lee JH, Kim YT, Riu DH, Jung SJ, Lee YJ, et al. Synthesis of Si, Mg substituted hydroxyapatites and their sintering behaviors. *Biomaterials* 2003;24:1389-98.
- [20] Ruys AJ. Silicon-doped hydroxyapatite. *Journal of the Australian ceramic society* 1993;29:71-80.
- [21] Putlayev V, Veresov A, Pulkin M, Soin A, Kuznetsov V. Silicon-substituted hydroxyapatite ceramics (Si-HAP): densification and grain growth through the prism of sintering theories. *Materials Science and Engineering Technology* 2006;37:416-21.
- [22] Best SM, Zou S, Brooks RA, Huang J, Rushton N, Bonfield W. The osteogenic behaviour of silicon substituted hydroxyapatite. *Key Engineering Materials* 2008;361-363:985-8.
- [23] Hing KA, Revell PA, Smith N, Buckland T. Effect of silicon level on rate, quality and progression of bone healing within silicate-substituted porous hydroxyapatite scaffolds. *Biomaterials* 2006;27:5014-26.
- [24] Bothelo CM, Brooks RA, Best SM, Lopes MA, Santos JD, Rushton N, et al. Human osteoblast response to silicon-substituted hydroxyapatite. *Journal of Biomedical Materials Research* 2006;79A:723-30.
- [25] Thian ES, Huang J, Best SM, Barber ZH, Brooks RA, Rushton N, et al. The response of osteoblasts to nanocrystalline silicon-substituted hydroxyapatite thin films. *Biomaterials* 2006;27:2692-8.
- [26] Hing KA, Wilson LF, Buckland T. Comparative performance of three ceramic bone graft substitutes. *The Spine Journal* 2007;7:475-90.
- [27] Palard M, Combes J, Champion E, Foucaud S, Rattner A, Bernache-Assollant D. Effect of silicon content on the sintering and biological behaviour of $\text{Ca}_{10}(\text{PO}_4)_{6-x}(\text{SiO}_4)_x(\text{OH})_{2-x}$ ceramics. *Acta Biomaterialia* 2009;5:1223-32.
- [28] Boanini E, Gazzano M, Bigi A. Ionic substitutions in calcium phosphates synthesized at low temperature. *Acta Biomaterialia* 2010;6:1882-94.
- [29] Bohner M. Silicon-substituted calcium phosphates – A critical view. *Biomaterials* 2009;30:6403-6.
- [30] Gomes S, Renaudin G, Mesbah A, Jallot E, Bonhomme C, Babonneau F, et al. Thorough analysis of silicon substitution in biphasic calcium phosphate bioceramics: A multi-technique study. *Acta Biomaterialia* 2010;6:3264-74.
- [31] Langstaff S, Sayer M, Smith TJN, Pugh SM. Resorbable bioceramics based on stabilized calcium phosphates. Part II: evaluation of biological response. *Biomaterials* 2001;22:135-50.
- [32] Palard M, Champion E, Foucaud S. Synthesis of silicated hydroxyapatite $\text{Ca}_{10}(\text{PO}_4)_{6-x}(\text{SiO}_4)_x(\text{OH})_{2-x}$. *Journal of Solid State Chemistry* 2008;181:1950-60.
- [33] Pietak AM, Reid JW, Sayer M. Electron spin resonance in silicon substituted apatite and tricalcium phosphate. *Biomaterials* 2005;26:3819-30.
- [34] Reid JW, Tuck L, Sayer M, Fargo K, Hendry JA. Synthesis and characterization of single-phase silicon-substituted α -tricalcium phosphate. *Biomaterials* 2006;27:2916-25.

- [35] Tang Q, Brooks RA, Rushton N. Production and characterization of HA and SiHA coatings. *Journal of Materials Science: Materials in Medicine* 2010;21:173-81.
- [36] Arcos D, Rodríguez-Carvajal J, Vallet-Regí M. Silicon incorporation in hydroxyapatite obtained by controlled crystallization. *Chemistry of materials* 2004;16:2300-8.
- [37] Balas F, Pérez-Pariente J, Vallet-Regí M. *In vitro* bioactivity of silicon-substituted hydroxyapatites. *Journal of Biomedical Materials Research Part A* 2003;66A:364-75.
- [38] Kanaya T, Tsuru K, Hayakawa S, Osaka A, Fujii E, Kowabata K, et al. Structure and *in vitro* solubility of silicon-substituted hydroxyapatite. *Key Engineering Materials* 2008;361-363:63-6.
- [39] Botelho CM, Lopes MA, Gibson IR, Best SM, Santos JD. Structural analysis of Si-substituted hydroxyapatite: zeta potential and X-ray photoelectroscopy. *J Mat Sc* 2002;13:1123-7.
- [40] Bothelo CM, Brooks RA, Best SM, Lopes MA, Santos JD, Rushton N, et al. Biological and physical-chemical characterization of phase pure HA and Si-Substituted Hydroxyapatite by different microscopy techniques. *Key Engineering Materials* 2004;254-256:845-8.
- [41] Bothelo CM, Brooks RA, Kawai T, Ogata S, Ohtsuki C, Best SM, et al. *In vitro* analysis of protein adhesion to phase pure hydroxyapatite and silicon substituted hydroxyapatite. *Key Engineering Materials* 2005;284-286:461-4.
- [42] Bothelo CM, Brooks RA, Spence G, I. M, Lopes MA, Best SM, et al. Differentiation of mononuclear precursors into osteoclasts on the surface of Si-Substituted hydroxyapatite. *Journal of biomedical Materials research part A* 2006;78A:709-20.
- [43] Bothelo CM, Stokes DJ, Brooks RA, Best SM, Lopes MA, Santos JD, et al. Effect of the human serum proteins on pure hydroxyapatite and silicon substituted hydroxyapatite: AFM and SEM studies. *Materials Science Forum* 2004;455-456:378-82.
- [44] Gibson IR, Best SM, Bonfield W. Effect of Silicon substitution on the sintering and microstructure of hydroxyapatite. *Journal of the American Ceramic Society* 2002;85:2771-7.
- [45] Gupta G, Kirakodu S, El-Ghannam A. Dissolution kinetics of a Si-rich nanocomposite and its effect on osteoblast gene expression. *Journal of Biomedical Materials Research* 2006;80A:486-96.
- [46] Guth K, Campion C, Buckland T, Hing KA. Effect of Silicate-Substitution on Attachment and Early Development of Human Osteoblast-Like Cells Seeded on Microporous Hydroxyapatite Discs. *Advanced Engineering Materials* 2010;12:1527-2648.
- [47] Guth K, Campion C, Buckland T, Hing KA. Effects of serum protein on ionic exchange between culture medium and microporous hydroxyapatite and silicate-substituted hydroxyapatite. *Journal of Materials Science: Materials in Medicine* 2011;22:2155-64.
- [48] Hijón N, Victoria Cabañas M, Peña J, Vallet-Regí M. Dip coated silicon-substituted hydroxyapatite films. *Acta Biomaterialia* 2006;2:567-74.
- [49] Lehmann G, Palmero P, Cacciotti I, Pecci R, Campagnolo L, Bedini R, et al. Design production and biocompatibility of nanostructured porous HAp and SiHAp ceramics as three dimensional scaffolds for stem cell culture and. *Ceramics – Silikáty* 2010;54:90-6.
- [50] Leventouri T, Bunaciu CE, Perdikatsis V. Neutron powder diffraction studies of silicon-substituted hydroxyapatite. *Biomaterials* 2003;24:4205-11.

- [51] López-Álvarez M, Solla EL, González P, Serra J, León B, Marques AP, et al. Silicon–hydroxyapatite bioactive coatings (Si–HA) from diatomaceous earth and silica. Study of adhesion and proliferation of osteoblast-like cells. *Journal of Materials Science: Materials in Medicine* 2009;20:1131-6.
- [52] Martinez IM, Velasquez PN, De Aza PN. Synthesis and stability of α -tricalcium phosphate doped with dicalcium silicate in the system $\text{Ca}_3(\text{PO}_4)_2\text{-Ca}_2\text{SiO}_4$. *Materials Characterization* 2010;61:761-7.
- [53] Porter AE, Patel N, Skepper JN, Best SM, Bonfield W. Comparison of *in vivo* dissolution processes in hydroxyapatite and silicon-substituted hydroxyapatite bioceramics. *Biomaterials* 2003;24:4609-20.
- [54] Seet SL. Silicon-substituted calcium phosphate compounds - Synthesis characterization and biological evaluation (Fumed silica). *Science Asia* 2009;35:255-60.
- [55] Marques da Silva H, Mateescu M, Ponche A, Damia C, Champion E, Soares G, et al. Surface transformation of silicon-doped hydroxyapatite immersed in culture medium under dynamic and static conditions. *Colloids and Surfaces B: Biointerfaces* 2010;75:349-55.
- [56] Sprio S, Tampieri A, Landi E, Sandri M, Martorana S, Celotti G, et al. Physico-chemical properties and solubility behaviour of multi-substituted hydroxyapatite powders containing silicon. *Materials Science and Engineering: C* 2008;28:179-87.
- [57] Vandiver J, Dean D, Patel N, Botelho C, Best SM, Santos JD, et al. Silicon addition to hydroxyapatite increases nanoscale electrostatic, van der Waals, and adhesive interactions. *Journal of Biomedical Materials Research Part A* 2006;78A:352-63.
- [58] Zou S, Ireland D, Brooks RA, Rushton N, Best S. The effects of silicate ions on human osteoblast adhesion, proliferation, and differentiation. *Journal of Biomedical Materials Research Part B: Applied Biomaterials* 2009;90B:123-30.
- [59] Arcos D, Sanchez-Salcedo S, Izquierdo-Barba I, Ruiz L, Gonzalez-Calbet J, Vallet-Regí M. Crystallochemistry, textural properties, and *in vitro* biocompatibility of different silicon-doped calcium phosphates. *Journal of Biomedical Materials Research* 2006;78A:762-71.
- [60] Bakunova N, Fomin A, Fadeeva I, Barinov S, Shvorneva L. Silicon-containing hydroxylapatite nanopowders. *Russian Journal of Inorganic Chemistry* 2007;52:1492-7.
- [61] Thian ES, Huang J, Best SM, Barber ZH, Bonfield W. Silicon-substituted hydroxyapatite: The next generation of bioactive coatings. Symposium A: Advanced Biomaterials International Conference on Materials for Advanced Technologies (ICMAT 2005) 2007;27:251-6.
- [62] Huang T, Xiao Y, Wang S, Huang Y, Liu X, Wu F, et al. Nanostructured Si Mg CO_3 Hydroxyapatite Coatings Deposited by Liquid Precursor Plasma Spraying. *Journal of the thermal spray technology* 2011;20:829-36.
- [63] Gillespie P, Wu G, Sayer M, Stott MJ. Si complexes in calcium phosphate biomaterials. *Journal of Materials Science: Materials in Medicine* 2010;21:99-108.
- [64] Langstaff S, Sayer M, Smith TJN, Pugh SM, Hesp SAM, Thompson WT. Resorbable bioceramics based on stabilized calcium phosphates. Part I: rational design, sample preparation and material characterization. *Biomaterials* 1999;20:1727-41.
- [65] Reid JW, Pietak A, Sayer M, Dunfield D, Smith TJN. Phase formation and evolution in the silicon substituted tricalcium phosphate/apatite system. *Biomaterials* 2005;26:2887-97.

- [66] Sayer M, Stratilatov AD, Reid J, Calderin L, Stott MJ, Yin X, et al. Structure and composition of silicon-stabilized tricalcium phosphate. *Biomaterials* 2003;24:369-82.
- [67] Borsa R-N. Elaboration de poudres et de dépôts de phosphates de calcium silicatés à usage de biomatériaux. Toulouse: Université de Toulouse; 2008.
- [68] Aminian A, Solati-Hashjin M, Samadikuchaksaraei A, Bakhshi F, Gorjipour F, Farzadi A, et al. Synthesis of silicon-substituted hydroxyapatite by a hydrothermal method with two different phosphorous sources. *Ceramics International* 2011;37:1219-29.
- [69] Kim YH, Song H, Riu DH, Kim SR, Kim HJ, Moon JH. Preparation of porous Si-incorporated hydroxyapatite. *Current Applied Physics* 2005;5:538-41.
- [70] Tian T, Jiang D, Zhang J, Lin Q. Synthesis of Si-substituted hydroxyapatite by a wet mechanochemical method. *Materials Science and Engineering: C* 2008;28:57-63.
- [71] Solla EL, Gonzalez P, Serra J, Chuiussi S, Leon B, Garcia Lopez J. Pulsed laser deposition of silicon substituted hydroxyapatite coatings from synthetical and biological sources. *Applied Surface Science* 2007;254:1189-93.
- [72] Xiao XF, Liu RF, Tang XL. Electrophoretic deposition of silicon substituted hydroxyapatite coatings from n-butanol-chloroform mixture. *Journal of Materials Science: Materials in Medicine* 2008;19:175-82.
- [73] Panteix P-J, Bécahde E, Julien I, Abélard P, Bernache-Assollant D. Influence of anionic vacancies on the ionic conductivity of silicated rare earth apatites. *Materials Research Bulletin* 2008;43:1223-31.
- [74] Bianco A, Cacciotti I, Lombardi M, Montanaro L. Si-substituted hydroxyapatite nanopowders: Synthesis, thermal stability and sinterability. *Materials Research Bulletin* 2009;44:345-54.
- [75] Porter AE, Patel N, Skepper JN, Best SM, Bonfield W. Effect of sintered silicate-substituted hydroxyapatite on remodelling processes at the bone-implant interface. *Biomaterials* 2004;25:3303-14.
- [76] Marques PAAP, Magalhaes MCF, Correia RN, Vallet-Regí M. Synthesis and characterization of silicon-substituted hydroxyapatite. *Key Engineering Materials* 2001;192-195:247-50.
- [77] Plokhikh NV, Soin AV, Kuznetsov AV, Veresov AG, Putlayev VI, Tretyakov YD. Synthesis of silico-substituted hydroxyapatite. *Mendelev Communications* 2004;14:178-9.
- [78] Mostafa NY, Hassan HM, Abd Elbader OH. Preparation and Characterization of Na^+ , SiO_4^{4-} , and CO_3^{2-} , Co-Substituted Hydroxyapatite. *Journal of the American Ceramic Society* 2011;94:1584-90.
- [79] Mostafa NY, Hassan HM, Mohamed FH, Omar H. Preparation of Na^+ , SiO_4^{4-} and CO_3^{2-} co-substituted hydroxyapatite nanoparticles. *Materials Research Bulletin* 2009;In Press, Accepted Manuscript.
- [80] Klein LC, Woodman RH. Porous silica by the Sol-Gel Process. *Key Engineering Materials* 1996;115:109-24.
- [81] Elliott JC. Structure and Chemistry of the Apatites and Other Calcium Orthophosphates. Amsterdam-London-New York-Tokyo: Elsevier; 1994.

- [82] Sefcik J, McCormick V. Thermochemistry of aqueous silicate solution precursors to ceramics. *Ceramics Processing* 1997;43:2773-84.
- [83] Lafon JP, Champion E, Bernache-Assollant D. Processing of AB-type carbonated hydroxyapatite $\text{Ca}_{10-x}(\text{PO}_4)_6-x(\text{CO}_3)_x(\text{OH})_{2-x-2y}(\text{CO}_3)_y$ ceramics with controlled composition. *Journal of the European Ceramic Society* 2008;28:139-47.
- [84] Rey C, Collins B, Goehl T, Dickson IR, Glimcher MJ. The carbonate environment in bone mineral: a resolution enhanced Fourier transform infrared spectroscopy study. *Calcified Tissue International* 1989;45:157-64.
- [85] Mostafa NY, Hassan HM, Mohamed FH. Sintering behavior and thermal stability of Na^+ , SiO_4^{4-} and CO_3^{2-} co-substituted hydroxyapatites. *Journal of Alloys and Compounds* 2009;479:692-8.
- [86] Marchat D, Bernache-Assollant D, Champion E. Cadmium fixation by synthetic hydroxyapatite in aqueous solution - Thermal behaviour. First International Conference on Engineering for Waste Treatment: Beneficial Use of Waste and By-Products (WasteEng2005) 2007;139:453-60.
- [87] Stadelmann P. Java Electron Microscopy Simulation (JEMS) software. Switzerland: CIME-EPFL, École Polytechnique Fédérale de Lausanne; 1999-2006.
- [88] Miquel JL, Facchini L, Legrand AP, Marchandise X, Lecouffe P, Chanavaz M, et al. Characterization of bioacceptable carbon materials. *Clinical Materials* 1990;5:115-25.
- [89] Hartmann P, Barth S, Vogel J, Meyer K. Solid State NMR, X-Ray Diffraction, and Infrared Characterization of Local Structure in Heat-Treated Oxyhydroxyapatite Microcrystals: An Analog of the Thermal Decomposition of Hydroxyapatite during Plasma-Spray Procedure *Journal of Solid State Chemistry* 2001;160:460-8.
- [90] Bonhomme C, Babonneau F, Azaïs T, Coelho C, Aimé C, Quignard S, et al. Dynamic Nuclear Polarization (DNP) for the characterization of nanoparticles. *The Journal of Physical Chemistry* 2012;(Submitted).
- [91] Arends J, Christoffersen J, Christoffersen MR, Eckert H, Fowler BO, Heughebaert JC, et al. A calcium hydroxyapatite precipitated from an aqueous solution. *Journal of Crystal Growth* 1987;84.
- [92] Rey C, Shimizu M, Collins B, Melvin JG. Resolution-enhanced Fourier transform infrared spectroscopy study of the environment of phosphate ions in the early deposits of a solid phase of calcium-phosphate in bone and enamel, and their evolution with age. 1: Investigations in the $n_4 \text{PO}_4$ Domain. *Calcified Tissue International* 1990;46:384-94.
- [93] Park E, Condrate SRA, Lee D, Kociba K, Gallagher PK. Characterization of hydroxyapatite: before and after plasma spraying. *Journal of Materials Science* 2002;13:211-8.
- [94] Rey C, Shimizu M, Collins B, Glimcher J. Resolution-enhanced Fourier transform infrared spectroscopy study of the environment of phosphate ions in the early deposits of a solid phase of calcium-phosphate in bone and enamel, and their evolution with age. 2: Investigations in the $n_3 \text{PO}_4$ Domain. *Calcified Tissue International* 1991;49:383-8.
- [95] Zymelka M, Marchat D, Szenknect S, Dacheux N, Bernache-Assollant D, Chevalier J. Silicon-substituted hydroxyapatite particles precipitation and dissolution. *Acta Biomaterialia* 2012;(Submitted).

- [96] Jillavenkatesa A, Condrate RA. The infrared and Raman spectra of b and a tricalcium phosphate ($\text{Ca}_3(\text{PO}_4)_2$). Spectroscopy letters 1998;31:1619-34.
- [97] Sanger AT, F. K. Structural disorder in hydroxyapatite. Zeitschrift fur Kristallographie 1992;199:123-48.
- [98] Hamilton WC, Ibers JA. Hydrogen Bonding in Solids. WA Benjamin : New-York 1968:204-21.
- [99] Liao C-J, Lin F-H, Chen K-S, Sun J-S. Thermal decomposition and reconstitution of hydroxyapatite in air atmosphere. Biomaterials 1999;20:1807-13.
- [100] Radin SR, Duchyene P. Plasma spraying induced changes of calcium phosphate ceramic characteristics and the effect on *in vitro* stability. Journal of Materials Science: Materials in Medicine 1992;3:33-42.
- [101] Trombe J-C. Mise en vidence d'oxygene  differents degres d'oxydation dans le rseau des apatites phosphocalciques et phosphostrontiques,. Annales de Chime 1973;8:335-47.
- [102] Trombe J-C, Montel G. Some features of the incorportaion of oxygen in different oxidation states in the apatitic lattice - II on the synthesis and properties of calcium and strontium peroxiapatites
Journal of Inorganic and Nuclear Chemistry 1978;40:23-6.
- [103] Wang T, Dorner-Reisel A, Muller E. Thermogravimetric and thermokinetic invetsigation of the dehydroxylation of hydroxyapatite powder. Journal of the European Ceramic Society 2004;24:693-8.
- [104] Bernache-Assollant D, Ababou A, Champion E, Heughebaert M. Sintering of calcium phosphate hydroxyapatite $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$, I. Calcination and particle growth. Journal of the European Ceramic Society 2003;23:229-41.
- [105] Liu Y, Shen Z. Dehydroxyalation of hydroxyapatite in dense bulk ceramics sintered by spark plasma sintering. ECERS 2012;32:2691-6.
- [106] Trombe J-C, Montel G. Some features of the incorporation of oxygen in different oxidation states in the apatitic lattice - I. On the existence of calcium and strontium oxyapatite. Journal of Inorganic and Nuclear Chemistry 1978;40:15-21.
- [107] Seuter AMJH. Existence Region of Calcium Hydroxyapatite and the
Equilibrium with Coexisting Phases at Elevated Temperatures. In: Anderson J.S RMW, Stone F.S., editor. Reactivity
of Solids1972.
- [108] Heughebaert JC. Contribution  l'tude de l'volution des orthophosphates de calcium prcipits amorphes en orthophosphates apatitiques [Sciences physiques]. Toulouse: Institut National Polytechnique; 1977.
- [109] Heughebaert JC, Montel G. tude de l'volution de l'orthophosphate tricalcique non cristallin en phosphate apatitique  la faveur d'une raction chimique  temprature ordinaire. Revue de Physique Applique 1977;12:691-4.
- [110] Aguiar H, Serra J, Gonzalez P, Leon B. Structural study of sol–gel silicate glasses by IR and Raman spectroscopies. Journal of Non-Crystalline Solids 2009;355:475-80.

- [111] Guerrero A, Goni S, A. M, Dolado JS. Microstructure and mechanical performance of Belite cements from high calcium coal fly ash. *Journal of American Ceramic Society* 2005;88:1845-53.
- [112] Hollenstein C, Howling AA, Courteille C, Magni D, M. SS, Kroesen GMW, et al. Silicon oxide particle formation in RF plasmas investigated by infrared absorption spectroscopy and mass spectrometry. *Journal of Physics D: Applied Physics* 1998;31:74-84.
- [113] Dunfield D, Sayer M, Shurvell HF. Total Attenuated Reflection Infrared Analysis of Silicon-Stabilized Tri-Calcium Phosphate. *The Journal of Physical Chemistry B* 2005;109:19579-19583.
- [114] Al-Oweini R, El-Rassy H. Synthesis and characterization by FTIR spectroscopy of silica aerogels prepared using several Si(OR)_4 and R''Si(OR')_3 precursors. *Journal of Molecular Structure* 2009;919:140-5.
- [115] Fidalgo A, Ilharco LM. The defect structure of sol-gel derived silica/polytetrahydrofuran hybrid films by FTIR. *Journal of Non-Crystalline Solids* 2001;283:144-54.
- [116] Gopal NO, Narasimhulu KV, Rao JL. EPR, optical, infrared and Raman spectral studies of Actinolite mineral. *Spectrochimica Acta* 2004;60:2441-8.
- [117] Alekhina LG, Akhmanova MV, Dement'ev VA, Gribov LA. Solution of the inverse spectroscopic problem for the SiO_4 group. *Journal of Applied Spectroscopy* 1975;22:546-9.
- [118] Bensted J, Varma SP. Some applications of infrared and Raman spectroscopy in cement chemistry. Part 2 - Portland cement and its constituents. *Cement Technology* 1974;4:378-82.
- [119] Dutta PK, Shieh D-C. Raman Spectral Study of the composition of basic silicate solutions. *Applied Spectroscopy* 1985;39:343-6.
- [120] Etchepare J. Interprétation des spectres de diffusion Raman de verres de silice binaires. *Spectrochimica Acta* 1970;26A:2147-54.
- [121] Mollah MYA, Yu W, Schennach R, Cocke DL. A fourier transform infrared spectroscopic investigation of the early hydration of Portland cement and the influence of sodium lignosulfonate. *Cement and concrete research* 2000;30:267-73.
- [122] Nakamura M, Mochizuki Y, usami K, Y. I, T. N. Infrared absorption spectra and compositions of evaporated silicon oxides (SiO_x). *Solid State Communications* 1984;50:1079-81.
- [123] Theil JA, Tsu DV, Watkins MW, Kim SS, Lucovsky G. Local bonding environment of Si-OH groups in SiO_2 deposited by remote plasma-enhanced chemical vapor deposition and incorporated by postdeposition exposure to water vapor. *American Vacuum Society* 1990;A8:1374-81.
- [124] Socrates G. Infrared and Raman characteristic group frequencies : Tables and Charts 2004.
- [125] Bell RJ, Bird NF, Dean P. The vibrational spectra of vitreous silica, germania and beryllium fluoride *Journal of Physics C: Solid State Physics* 1968;1:299-303.
- [126] Sato RK, McMillan PF. An infrared and Raman study of the isotopic species of alpha-quartz. *The Journal of Physical Chemistry B* 1987;91:3494-8.

- [127] Sitarz M, Handke M, Mozgawa W. Identification of silicoxygen rings in SiO_2 based on IR spectra. *Spectrochimica Acta Part A: Molecular and Biomolecular Spectroscopy* 2000;56:1819-23.
- [128] Ahsan MR, Mortuza MG. Infrared spectra of $x\text{CaO}(1-x-z)\text{SiO}_2 \cdot z\text{P}_2\text{O}_5$ glasses. *Journal of Non-Crystalline Solids* 2005;351:2333-40.
- [129] Bosomworth DR, Hayes W, Spray ARL, Watkins GD. Absorption of Oxygen in Silicon in the Near and the Far Infrared Proceedings of the Royal Society (London) 1970;317:133-52.
- [130] Sari SO, Hollingsworth-Smith P, Oona H. Near IR absorption in films of silicon containing oxygen. *Journal of Physics and Chemistry of Solids* 1978;39:857.

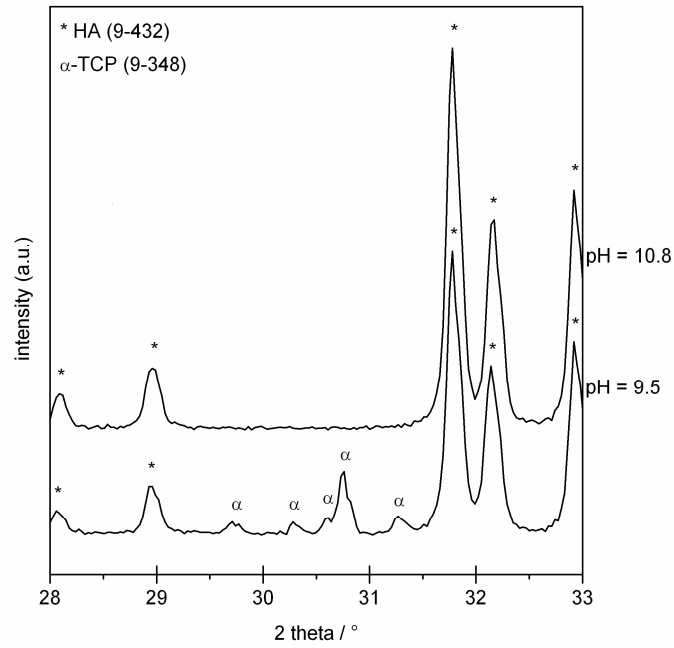


Fig. 1. XRD patterns of heat treated $\text{Si}_{0.50}\text{HA}$ powders prepared at 50°C and maintained at pH 9.5 and 10.8.

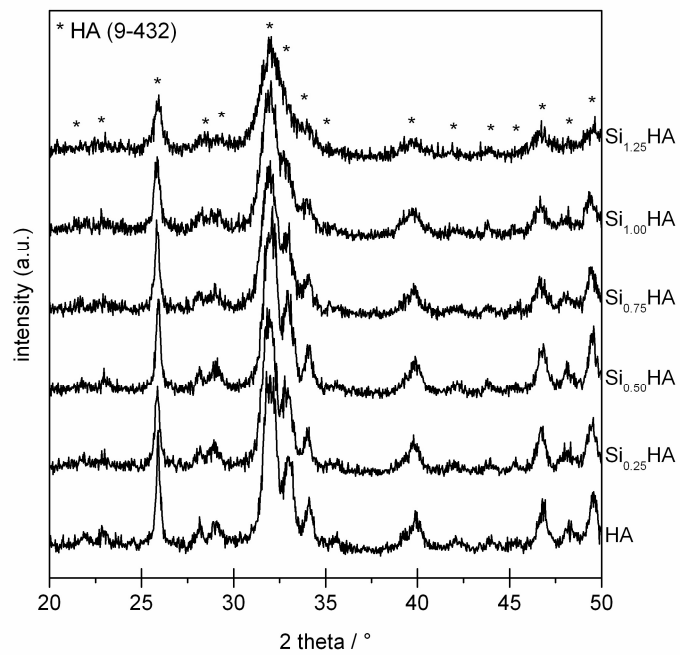


Fig. 2. X-ray diffraction patterns of raw SiHA powders synthesized at pH = 10.8 with different silicon concentration.

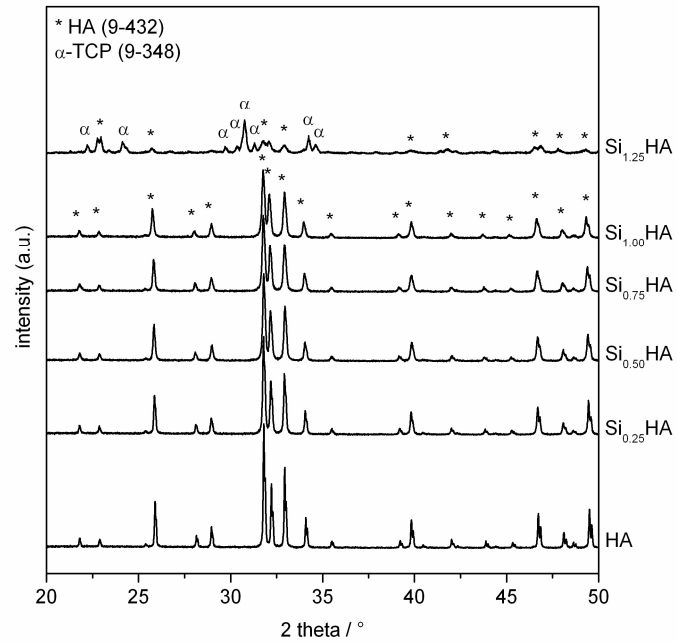


Fig. 3. X-ray diffraction patterns of heat treated (1000°C/15h) SiHA powders synthesized at pH = 10.8 with different silicon concentration.

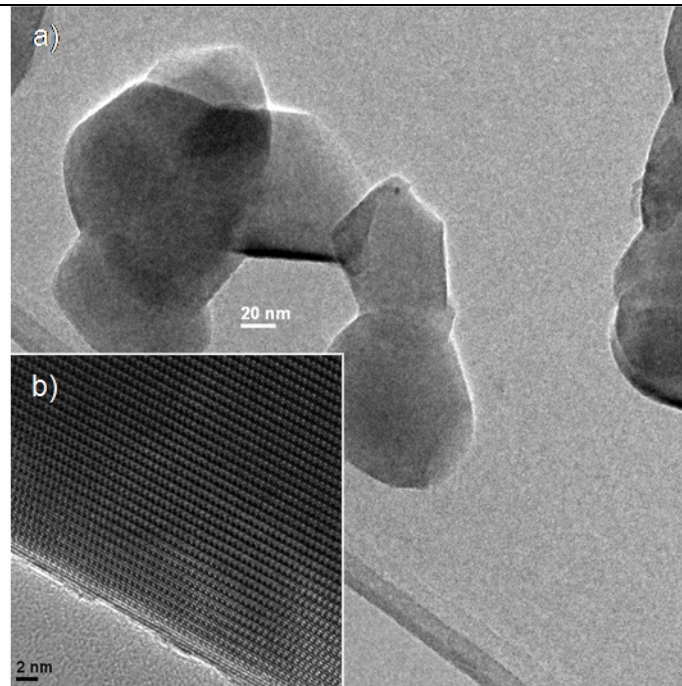


Fig. 4: (a) TEM micrograph of heat treated $\text{Si}_{1.0}\text{HA}$ crystallites (1000°C/15h), (b) High-resolution lattice image of a heat treated $\text{Si}_{1.0}\text{HA}$ particle (1000°C/15h) along the zone axis [01-1]; plane spacing of 8.2Å.

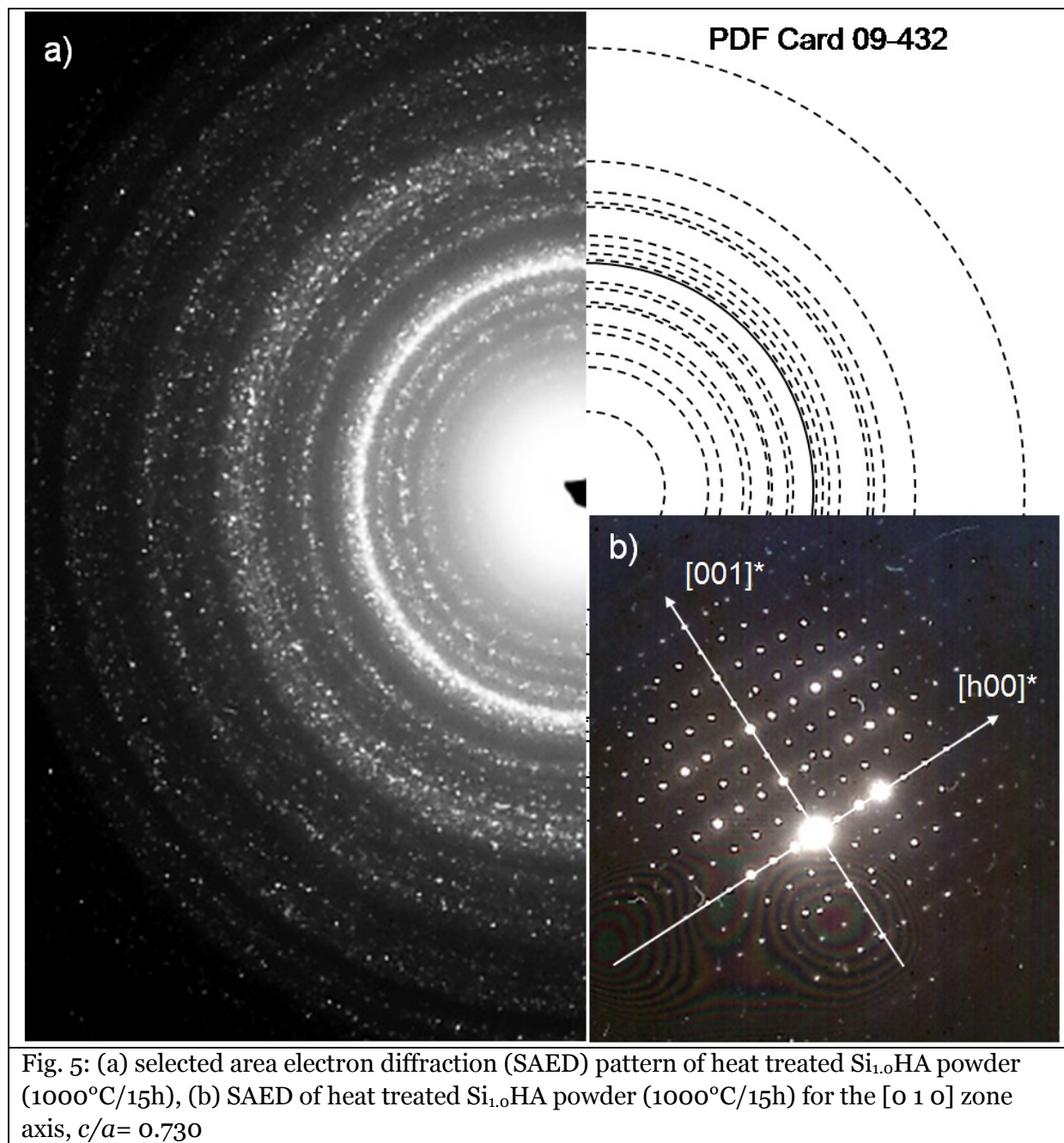


Fig. 5: (a) selected area electron diffraction (SAED) pattern of heat treated $\text{Si}_{1.0}\text{HA}$ powder (1000°C/15h), (b) SAED of heat treated $\text{Si}_{1.0}\text{HA}$ powder (1000°C/15h) for the $[0\ 1\ 0]$ zone axis, $c/a= 0.730$

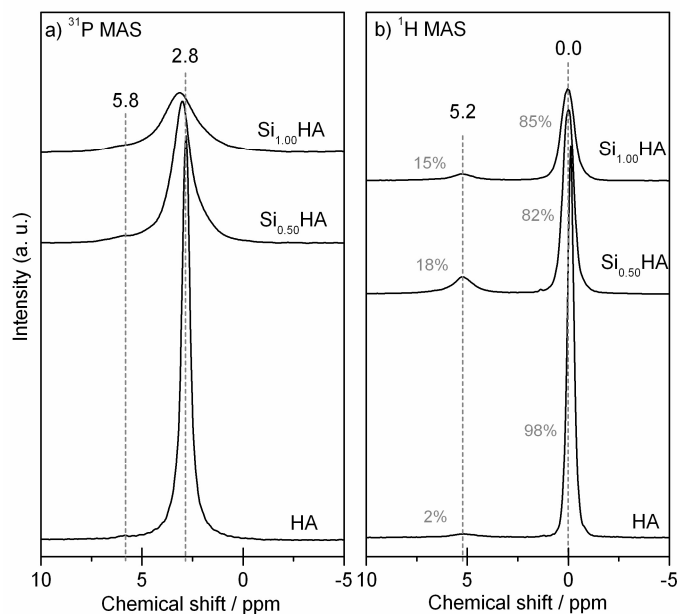


Fig. 6. (a) ^{31}P and (b) ^1H MAS-NMR spectra of the HA, $\text{Si}_{0.50}\text{HA}$ and $\text{Si}_{1.00}\text{HA}$ powders calcined at 1000°C for 15h.

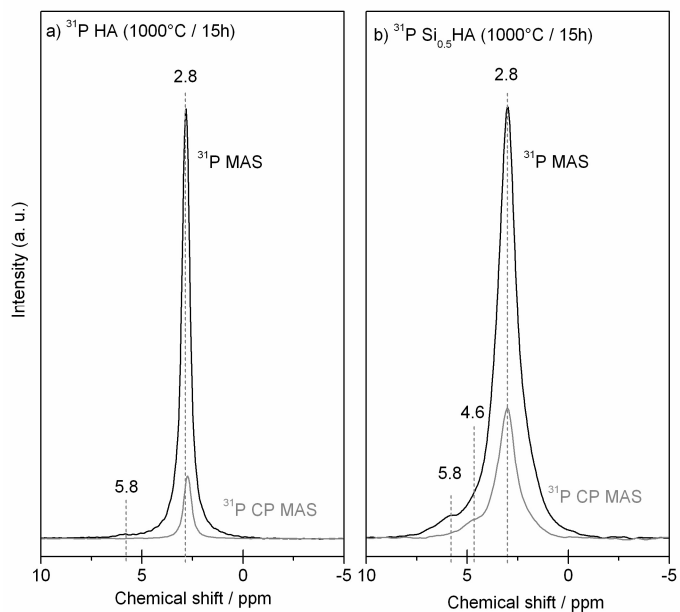


Fig. 7. Comparison between ^{31}P MAS-NMR and CP MAS NMR spectra of (a) HA and (b) $\text{Si}_{0.50}\text{HA}$ powders calcined at 1000°C for 15h.

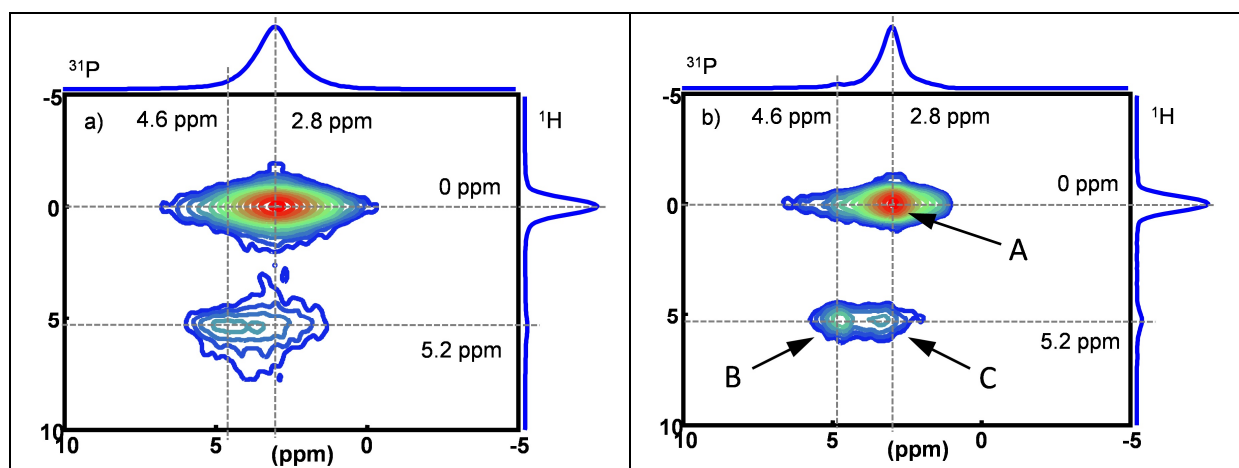


Fig. 8. ^1H - ^{31}P HETCOR CP MAS experiment recorded on (a) $\text{Si}_{1.00}\text{HA}$ powder calcined at 400°C for 2h, and (b) $\text{Si}_{0.50}\text{HA}$ powder calcined at 1000°C for 15h.

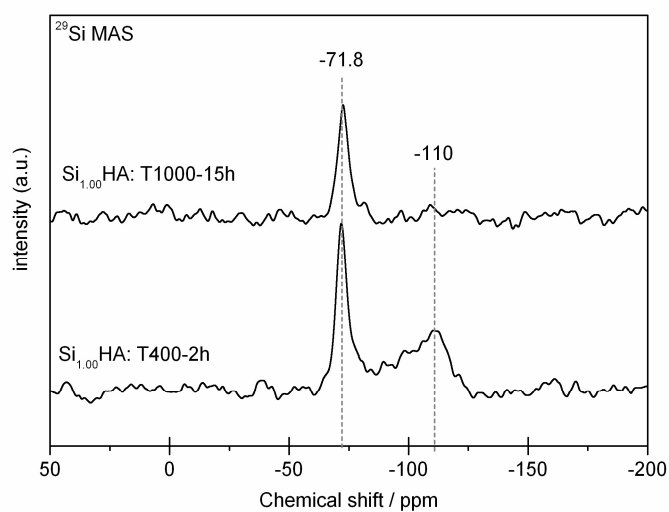


Fig. 9. ^{29}Si MAS-NMR spectra of the $\text{Si}_{1.00}\text{HA}$ powder calcined at 400°C for 2h and 1000°C for 15h

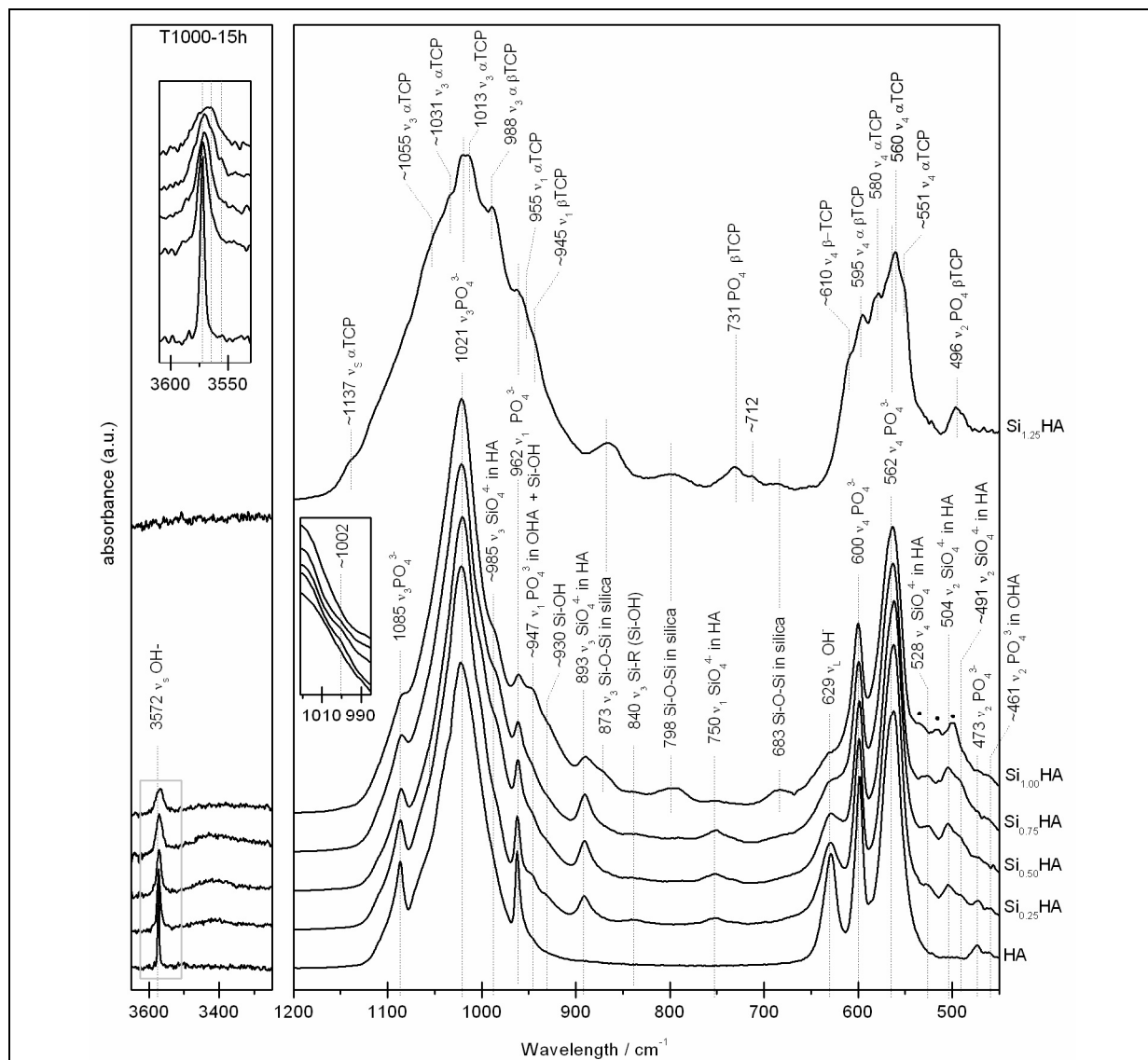


Fig. 10. FTIR spectra of calcined HA and SiHA powders (1000°C / 15h) collected at room temperature, symbol • shows additional vibrations for Si_{1.0}HA at 500, 515, 535 cm⁻¹.

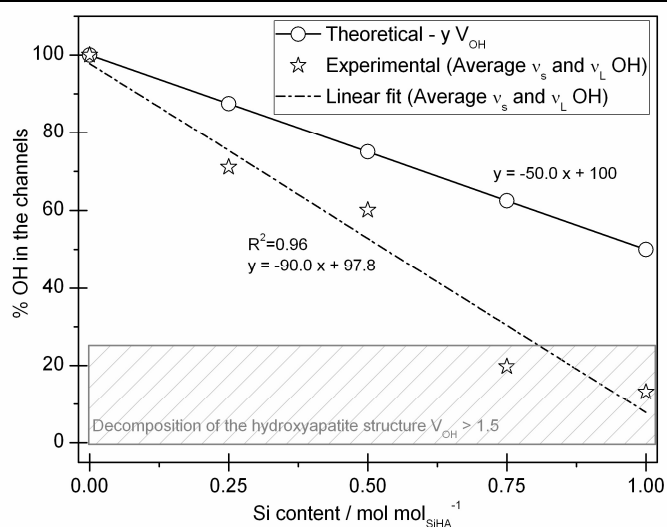


Fig. 11. OH content into the apatitic channels versus the Si content, for theoretical SiHA structure ($y V_{OH}$) and samples calcined at 1000°C for 15h (determined from integrated areas

of ν_L and ν_S bands).

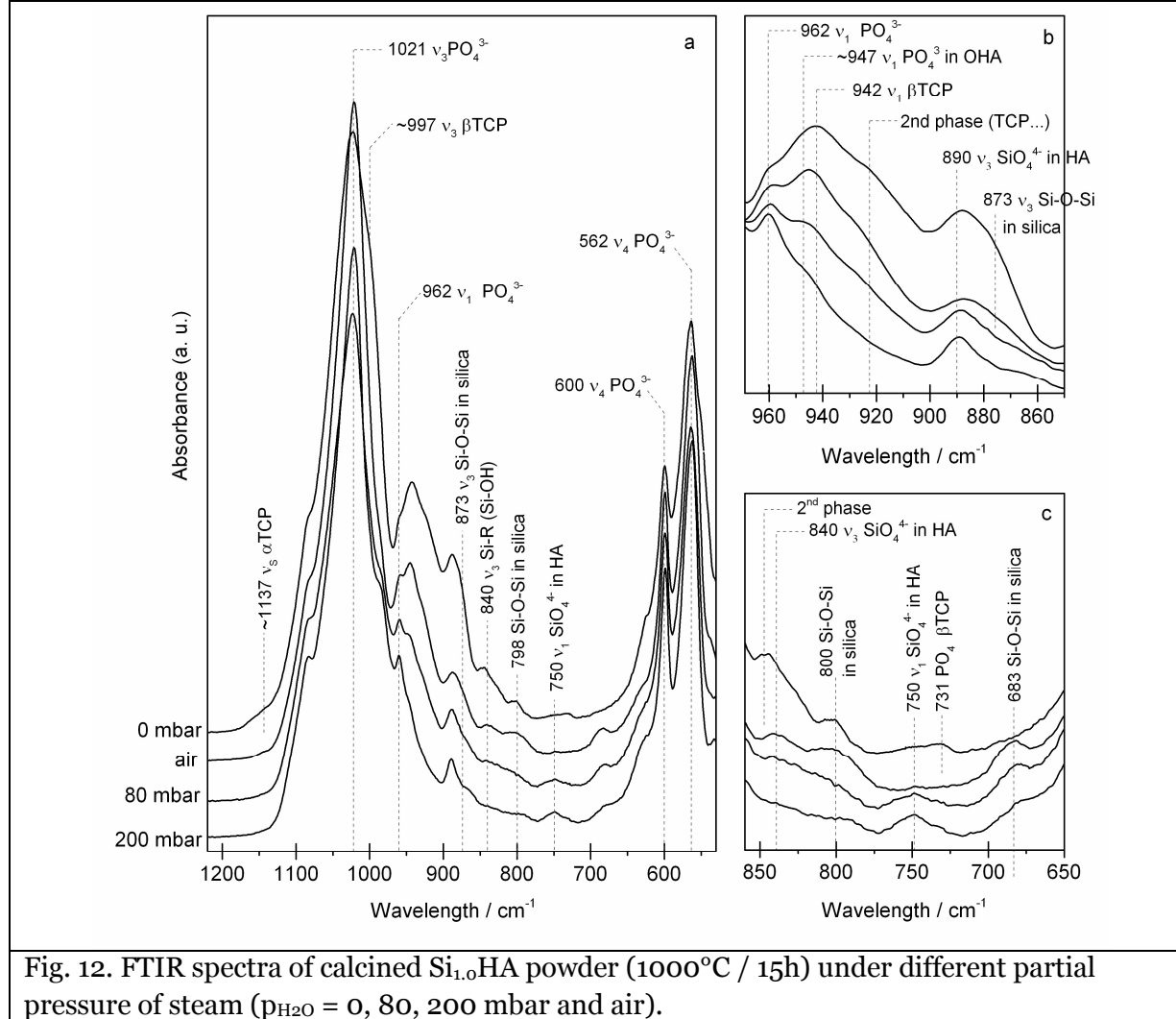


Fig. 12. FTIR spectra of calcined $\text{Si}_{1.0}\text{HA}$ powder (1000°C / 15h) under different partial pressure of steam ($p_{\text{H}_2\text{O}} = 0, 80, 200$ mbar and air).

Table 1

Chemical conditions of preparation of HA and Si_yHA samples and final composition of the calcined powders (1000°C/15h).

Sample	Synthesis parameters (T = 50°C, t _m =24h)					Composition of the final calcined powders (1000°C/15h)		
	n _{Ca}	n _P	n _{Si}	pH	y _{Si}	y _{Si}	Chemical formula of Si _y HA	Ca/(P+Si)
					Expected	Determined - According to Equation Eq. 2		Determined by ICP/AES
	/ mol	/ mol	/ mol	-	/ mol mol ⁻¹ _{SiHA}		-	
HA	0.200	0.120	0	9.5	0	0	Ca ₁₀ (PO ₄) ₆ (OH) ₂	1.69 ± 0.05
Si _{0.25} HA	0.200	0.115	0.005	11.0	0.25	0.28±0.02	Ca ₁₀ (PO ₄) _{5.72} (SiO ₄) _{0.28} (OH) _{1.72} (V _{OH}) _{0.28}	1.69 ± 0.02
Si _{0.50} HA	0.200	0.110	0.010	9.5	0.50	N/A	HA + α TCP	N/A
Si _{0.50} HA	0.200	0.110	0.010	11.0	0.50	0.52±0.02	Ca ₁₀ (PO ₄) _{5.48} (SiO ₄) _{0.52} (OH) _{1.48} (V _{OH}) _{0.52}	1.68 ± 0.02
Si _{0.75} HA	0.200	0.105	0.015	11.0	0.75	0.72±0.02	Ca ₁₀ (PO ₄) _{5.28} (SiO ₄) _{0.72} (OH) _{1.28} (V _{OH}) _{0.72}	1.67 ±0.03
Si _{1.00} HA	0.200	0.100	0.020	11.0	1.00	0.97±0.02	Ca ₁₀ (PO ₄) _{5.03} (SiO ₄) _{0.97} (OH) _{1.03} (V _{OH}) _{0.97}	1.67 ± 0.01
Si _{1.25} HA	0.200	0.095	0.025	11.0	1.25	N/A	HA+TCP	N/A

Table 2

NMR parameters.

NMR Experiments	t_{90°	number of scans	relaxation delay	^1H decoupling	contact time	t_1 increments
	/ μs	-	/ s	-	/ ms	
^1H MAS	4.6	4	300	-	-	-
^{31}P MAS	1.3	16	60	SPINAL-64 (54kHz)	-	-
^{31}P CPMAS	1.5	16	15		3	-
^1H - ^{31}P HETCOR CPMAS		32			1	128
^{29}Si MAS	1.5	~ 4000	60	SPINAL-64 (45kHz)	-	-

Table 3.

Lattice parameters, unit cell volume and mean size of the crystallites of heat-treated powders at 1000°C for 15h evaluated by Rietveld refinement.

Sample	Lattice parameters / Å		Volume of the unit cell / Å ³	Crystallites mean size / nm
	a-axis	c-axis		
PDF 9-432	9.418	6.884	1058	-
HA	$9.421 \pm 3 \cdot 10^{-5}$	$6.884 \pm 3 \cdot 10^{-5}$	1058 ± 1	243 ± 1
Si _{0,25} HA	$9.423 \pm 4 \cdot 10^{-5}$	$6.892 \pm 4 \cdot 10^{-5}$	1060 ± 1	157 ± 1
Si _{0,50} HA	$9.428 \pm 2 \cdot 10^{-4}$	$6.899 \pm 2 \cdot 10^{-4}$	1062 ± 1	116 ± 1
Si _{0,75} HA	$9.423 \pm 2 \cdot 10^{-4}$	$6.908 \pm 2 \cdot 10^{-4}$	1062 ± 1	103 ± 1
Si _{1,00} HA	$9.416 \pm 7 \cdot 10^{-5}$	$6.920 \pm 5 \cdot 10^{-5}$	1063 ± 1	107 ± 1

Table 4

IR bands and shoulders assignment proposed by our work

λ / cm^{-1}	Mode assignments proposed by this work	Literature support
1002*	Degenerated PO_4^{3-} asymmetric stretching (ν_3)	[94, 110]
985	Si-OH at SiHA surface / and/or / Si in SiHA	[110-112]
947	Oxyapatite	[93, 99, 100, 102, 113]
	Si-OH at SiHA surface	[114-116]
930**	Si-OH at SiHA surface / and/or / Si in SiHA	[114, 117-121]
893	Si in SiHA	[8, 113, 118]
873	Si in silica	[112, 113, 122, 123]
840	Si-R	[118, 124]
798	Si in silica	[34, 110, 112-115, 117, 120, 122, 125-127]
750	Si in SiHA	[32, 54, 74]
683	Si in silica	[113, 114, 116, 126, 127]
535	Si in silica	[128]
528	Si in SiHA	[111, 118, 121, 128]
515	Si in silica	[127-130]
504	Si in SiHA	[32, 56, 118]

* degeneration of the ν_3 PO_4^{3-} domain at 1020 cm^{-1} due to the SiO_4^{4-} in the environment of the phosphate ions

** degeneration of the band at 947 cm^{-1}